The Effect of Sodium Hyaluronate on Ligamentation and Biomechanical Property of Tendon in Repair of Achilles Tendon Defect with Polyethylene Terephthalate Artificial Ligament: A Rabbit Tendon Repair Model

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The Achilles tendon is the most common ruptured tendon of human body. Reconstruction with polyethylene terephthalate (PET) artificial ligament is recommended in some serious cases. Sodium hyaluronate (HA) is beneficial for the healing of tendon injuries. We aimed to determine the effect of sodium hyaluronate in repair of Achilles tendon defect with PET artificial ligament in an animal tendon repair model. Sixteen New Zealand White rabbits were divided into two groups. Eight rabbits repaired with PET were assigned to PET group; the other eight rabbits repaired with PET along with injection of HA were assigned to HA-PET group. All rabbits were sacrificed at 4 and 8 weeks postoperatively for biomechanical and histological examination. The HA-PET group revealed higher biomechanical property compared with the PET group. Histologically, more collagen tissues grew into the HA-PET group compared with PET group. In conclusion, application of sodium hyaluronate can improve the healing of Achilles tendon reconstruction with polyethylene terephthalate artificial ligament.

1. Introduction

The incidence of Achilles tendon rupture increased during the past few years [1]. In some serious cases, direct repair is impossible. In that case, reconstruction of the tendon is required. There are many methods to treat the Achilles tendon rupture, including autograft reconstruction [2, 3], allograft reconstruction [4], and artificial ligament reconstruction [5]. However, the autograft tendon has the donor site problem, while the allograft tendon may increase the risk of disease transfusion or immunological rejection.

Artificial ligament is frequently used in the reconstruction of ligament rupture management like anterior cruciate ligament reconstruction [6], acromioclavicular joint reconstruction [7], also the Achilles tendon reconstruction [5], etc. Artificial ligaments can promise a fast functional recovery and avoid complications. In addition, there are various treatments applied for helping the healing of tendon injuries such as platelet-rich plasma (PRP) [8, 9] and sodium hyaluronate (HA) [10]. Sodium hyaluronate (HA) is polysaccharide, which is found in all extracellular matrix of vertebrates and in some bacteria as well [11]. In this way, it may be helpful to the wound healing process by generating proper environment for growth, leading to the accumulation of several matrix proteins [12].

Based on the background before, we applied the sodium hyaluronate (Bausch & Lomb Freda Co., Ltd., Shandong, China) after the repair procedure of Achilles tendon defect with PET artificial ligament. The aim of this study was to analyze the effect of sodium hyaluronate on ligamentation and biomechanical property of tendon in repair of Achilles tendon defect with PET in a rabbit tendon repair model.

2. Materials and Methods

2.1. Experimental Design. The animal experiment was approved by the Animal Care and Use Committee of our college. Two groups were involved in this study; the group
treated with sodium hyaluronate (HA) was set as an experimental group, while another group untreated with sodium hyaluronate was prepared as a control group.

2.2. Animals. Total 16 fifteen-week-old male New Zealand White rabbits (mean weight 2.6 ± 0.2 kg) were randomly selected for experiments. In the study, 8 rabbits were assigned to the experimental group, while another 8 rabbits were used for the control group. Animals were sacrificed at the time points of weeks 4 (n = 4) and 8 (n = 4) after surgery for both the experimental group and the control group.

2.3. Preparation of PET Sheet. PET sheets (Figure 1) were taken from the Ligament Advanced Reinforcement System (LARS) ligament and then soaked in 75% alcohol solution to remove foreign material and contamination for 4 hours, cleaned with a large amount of deionized water and then dried in air for 24 hours [13, 14].

2.4. Operative Procedure. Anesthesia was induced by the intravenous administration of 3% pentobarbital (30 mg/kg) [13]. The animal was placed prone on the operating table. After preparation of skin and disinfection, a longitudinal skin incision was made. Then, two-thirds of vertical plane of the Achilles tendon was cut by scissors to create a partial tendon injury. To help the Achilles tendon to heal, the PET sheets were implanted into the defect to strengthen the tendon by number 5 Ethibond suture for traction. Then, the sutures were fixed firmly in the biomechanical analyzer. Care was taken to keep the longitudinal tendon samples parallel to the testing axis. After preconditioning, the ultimate load-to-failure was performed with the extension rate of 5 mm/min. The load-to-failure (N) and the stiffness (N/mm) were measured, while the load-distortion curve was recorded. For each sample, testing ends when the tendon ruptured.

2.5. Histological Analysis. Identically located longitudinal tendon samples (n = 1 tendon of each group at each time) were collected randomly from the injured and normal tendons [16]. After fixation in 10% formalin for 24 h, the tendon samples were washed, dehydrated, cleared, and embedded in paraffin wax. The samples were then sectioned into layers with a thickness of 5 um perpendicular to the longitudinal axis of the tendon using a microtome (SM2500, Leica) [17]. These sections were stained with hematoxylin and eosin (H&E) staining and Masson trichrome staining [18]. The slides were examined by light microscopy (Olympus Optical Co., Tokyo, Japan) for initial evaluation and photography [13, 16–18]. Two evaluators who performed the histological observation were blinded to treatment group of the sections.

2.6. Biomechanical Analysis. The repaired tendons (n = 3 tendons of each group at each time) were harvested after sacrifice and subjected to mechanical testing within 6 h, using a biomechanical analyzer (AGS-X 5kN, Shimadzu Co., Japan). The dimension of the test tendon sample is approximately 4 cm. And all the samples were prepared for testing without being frozen. Both ends of the tendon were sutured by number 5 Ethibond suture for traction. Then, the sutures were fixed firmly in the biomechanical analyzer. Care was taken to keep the longitudinal tendon samples parallel to the testing axis. After preconditioning, the ultimate load-to-failure was performed with the extension rate of 5 mm/min. The load-to-failure (N) and the stiffness (N/mm) were measured, while the load-distortion curve was recorded. For each sample, testing ends when the tendon ruptured.

2.7. Statistical Analysis. Results are presented as mean and standard deviation. The paired Student t-test was used to compare the experimental group with control group to determine the significant differences. If p < 0.05, the differences were considered significant statistically.

3. Results

3.1. Mechanical Examination Results. No tendon rupture occurred for all specimens of both 4 and 8 weeks. The most common failure mode is the slippage of rope from the test tendon. At 4 weeks, there was no statistically significant difference in the load-to-failure between the HA-PET group and the control group (171.7 ± 38.1 N for HA-PET group and 156.7 ± 12.7 N for controls; p > 0.05), while at 8 weeks there was also no statistically significant difference between two groups (175.3 ± 44.7 N for HA-PET group and 137 ± 65.8 N for controls; p > 0.05) (Figure 2). Similarly, at 4 weeks there was no statistically significant difference in the stiffness between the HA-PET group and the control group (4.2 ± 2.4 N/mm for HA-PET group and 2.1 ± 0.9 N/mm for controls; p > 0.05). Meanwhile at 8 weeks there was also no statistically significant about stiffness difference between two groups (4.5 ± 3.8 N/mm for HA-PET group and 2.1 ± 0.3 N/mm for controls; p > 0.05) (Figure 3).

3.2. Histological Results. Four weeks after surgery it appeared that there was no tissue surrounding the graft fibers in both the PET and HA-PET groups. After 8 weeks, thick collagen tissue with some vasculature covered the grafts in the HA-PET group, while there was little tissue infiltration of the graft fibers in the PET group (Figures 4 and 5). Some cells from the fibrous tissue infiltrated the graft site, and the collagen fibers tended to orient along the axis of the tendon.
4. Discussion

Achilles tendon is the most common ruptured tendon of our human body [19]. Reconstruction procedure must be taken using allograft, autograft, or artificial ligament for some serious cases if direct repair is impossible. Artificial ligaments like LARS can provide enough intensity, while it is not fully bioactive for ligamentization. Additional treatment like sodium hyaluronate (HA) can facilitate the process of graft healing including inflammation, cellular adhesion and proliferation, vascular proliferation and pruning, and collagen remodeling [20]. In this study, we are trying to find out the effect of sodium hyaluronate for Achilles tendon reconstruction using PET.

Sodium hyaluronate partly contributes to cell adhesion and growth as well as inflammation suppressing. In a previous study, Li et al. found out that polyethylene terephthalate (PET) artificial ligament grafts coated with sodium hyaluronate can enhance cell adhesion, facilitated cell growth, and suppressed the expression of inflammation-related genes relative to a pure PET graft for ACL reconstruction [21]. Another study done by Nakamura et al. demonstrated that HA possesses anti-inflammatory and antiadhesive activities in tendon and synovial fibroblasts derived from RCT [22]. In addition, Salamanna et al. find out that, after repeated peripatellar injections of HA to rats, a significantly higher proliferation rate and viability, along with increased synthesis of C-terminal-propeptide of type I collagen, fibronectin, aggrecan, tenascin-c, and matrix-metalloproteinase-3 show respect to control group [23]. In this study, the administration of HA improved collagen formation which is good for tendon healing. The molecular weight and the concentration of NaHA influence the rate of the elimination process from the tendon sheath after local injection [24]. There are investigations suggesting that the injection of high-molecular-weight NaHA in high concentrations around the tendons improves tendon healing and decreases adhesion formation [24–26]. In our study, the weight-average molecular weight of NaHA is within $6 \times 10^5 \sim 1.5 \times 10^6$ which improves tendon healing to a certain extent. There are several different explanations on the effects of NaHA. Some researchers find out that NaHA acts as a physical barrier around the repaired tendon location, while others suggest that the main effect of NaHA may be developed pharmacologically or physiologically [24–26]. However, the exact mechanism of effect of NaHA is not clear.

The histological results especially the Masson staining in this study show that sodium hyaluronate can facilitate new collagen formation. Li et al. suggest that PET graft...
coated with HA can enhance not only cell adhesion and proliferation but also stimulating collagen generation \[21\]. Oryan et al. demonstrated that, after surgical treatment of tendon rupture, application of sodium hyaluronate to the lesions can improve the density of collagen fibers, almost similar to the normal contra-lateral tendons. Ultrastructural morphometric analyses of the number, diameter (nm), and density (%) of the collagen fibrils show significant differences with control group on both the number and the diameter of collagen fibrils \[27\]. In another study Halici et al. suggested that, after 6 weeks of repetitive administration of HA during the rabbit tendon healing process, type IV collagen expression increased significantly, and they believe it is part of the angiogenesis along with the increase of VEGF \[28\].

In our experiment, the mean load-to-failure and stiffness of HA-PET group appeared higher than those of the PET group. However, there are no significant differences in the mechanical examination results both on the 4 weeks’ and 8 weeks’ terminal point. Deng et al. \[13\] investigated the feasibility of using adipose derived stem cells (ASCs) for engineered tendon repair in vivo in a rabbit Achilles tendon model, and they found no difference in tensile strength at 5 weeks but found significant difference at the time points of 12 weeks, 21 weeks, and 45 weeks. Some other studies also show treatment of HA strongly improved the biomechanical properties of the injured tendons and the ultimate strength \[10, 27\]. One conceivable possibility is that, unlike with the normal Achilles tendon, PET artificial ligament has much better characteristic of strength and stiffness, and injection of HA may not add significant improvement of biomechanical property to PET artificial ligament. Only 16 rabbits were investigated in our study, which may be somehow insufficient on sample size.

5. Conclusion

Collectively, the histological results of our study demonstrate that application of sodium hyaluronate can improve collagen formation, which is beneficial for the healing of Achilles tendon reconstruction with polyethylene terephthalate artificial ligament.

Competing Interests

The authors report that they have no conflict of interests.

Authors’ Contributions

Shengkun Li and Kui Ma contributed equally to this work.

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