Improved T-S Fuzzy Control for Uncertain Time-Delay Coronary Artery System

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Received 8 March 2019; Revised 22 April 2019; Accepted 24 April 2019; Published 16 May 2019

Academic Editor: Yong Xu

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This paper is based on the Takagi-Sugeno (T-S) fuzzy models to construct a coronary artery system (CAS) T-S fuzzy controller and considers the uncertainties of system state parameters in CAS. We propose the fuzzy model of CAS with uncertainties. By using T-S fuzzy model of CAS and the use of parallel distributed compensation (PDC) concept, the same fuzzy set is assigned to T-S fuzzy controller. Based on this, a PDC controller whose fuzzy rules correspond to the fuzzy model is designed. By constructing a suitable Lyapunov-Krasovskii function (LKF), the stability conditions of the linear matrix inequality (LMI) are exported. Simulation results show that the method proposed in this paper is correct and effective and has certain practical significance.

1. Introduction

Since Pecora and Caroll proposed chaotic synchronization in 1990 [1], synchronization control of chaotic systems has developed rapidly and has become one of the most important topics during the past 30 years [2–12]. Two chaotic systems synchronization of the main idea is to design a suitable controller, to make the state of the slave system track the status of the master system. In order to solve the synchronization problem of chaotic systems, many methods have been proposed, such as feedback control method [13, 14], continuous sliding mode method [15, 16], and fuzzy control method [17, 18]. Among them, the fuzzy control has attracted much attention because of its wide application and independent of the precise mathematical model of the controlled object and so on. Takagi-Sugeno (T-S) fuzzy model can provide the approximation of nonlinear features by fuzzy mixing of multiple local linear models with appropriate membership functions, by using fuzzy rules, the dynamic nonlinear systems are approximated to the set of the local linear input and output relation, and the whole fuzzy model is finally obtained by smoothing the set of the local linear model with the fuzzy piecewise membership function. In [19], the chaotic system is modeled as a T-S fuzzy system, and stable results are obtained, so it has been shown that the fuzzy control may provide a system effective frame for the nonlinear system control design. According to literature [20], we know that T-S fuzzy model has made remarkable achievements in solving complex nonlinear systems.

The vasospasms are the main cause of cardiocerebral vascular diseases. Once the blood vessels with the chaotic state, it will lead to the occurrence of cardiocerebral vascular diseases such as vasospasm. The main chaotic phenomenon of coronary artery is vasospasm. In order to understand the nonlinear characteristics of vasospasm and to control the occurrence of chaos, literature [21] proves that diseased vessels have the same behavior as normal vessels. In literature [22], a chaos suppression controller is designed based on variable structure control theory. Application of higher-order sliding mode adaptive controller is in reference [23]. They use a synchronization controller to synchronize the chaotic motion state of the diseased vessels to that of the normal vessels, so as to achieve the goal of treatment. However, there are some clinical factors, such as the effect of the body’s own time delay on drug absorption in patients with coronary artery disease after taking the drug, not been proposed in the literature [21–23].

In order to reduce the negative impact of time delay, we need to reduce the conservatism of the system and improve the performance of the system; many researchers...
have used the triple integral form of LKF to analyze the stability of various time-delays systems in recent years, such as Wirtinger-based integral inequality [24], Jensen’s inequality [25], and Wirtinger-based double integral inequality [26], and explain its effectiveness in reducing the conservativeness of stability criteria. Due to the method of literature [26] can be applied directly in finding lower bound of double integral, such as\[ \int_{t-	au}^{t} \int_{s}^{t} x^T(u)N\dot{x}(u)du ds (N > 0), \]
and the method of literature [24] cannot be applied directly in solving it. Therefore, literature [26] is more conservative than literature [24] when dealing with system stability analysis. In order to further reduce the conservativeness of system stability analysis, we study the stability of chaotic time-delay synchronous control systems by using the method in [26]. In addition, for solving complex nonlinear systems, we design a parallel distributed compensation (PDC) controller based on fuzzy model.

From the above discussion, this paper is to explore chaotic synchronization of uncertain CAS based on fuzzy models. A PDC synchronization controller for a class of uncertain CAS with time delay is proposed using T-S fuzzy. Using Wirtinger-based double integral inequality [26] and Moon et al’s inequality [27] can further reduce the conservativeness of CAS. It is show that the synchronization controller can synchronize the response system with the drive system, and the error system tends to zero.

The structure of the paper is as follows. Section 2 shows that the T-S fuzzy control problem formulation of the same class for time-delay uncertain CAS. Section 3 describes the design of T-S fuzzy synchronization controller. We design LKF and we can get the LMI by using the lemma mentioned in Section 4. Results of simulation are analyzed shown in Section 5. Finally, we will give a conclusion in Section 6.

2. System Description and Problem Analysis

In this paper, considering the normal uncertain CAS with time delay as the driving system, the rules of T-S fuzzy model can be described as follows.

**Rule I**

**IF** \( x_1(t) \) **is** \( M_{i_1} \)

**THEN** \( \dot{x}_m(t) = (A_1 + \Delta A)x_m(t) + (B_1 + \Delta B)x_m(t - h(t)) + E \cos(t) + u(t) \)  

\[ (1) \]

**Rule II**

**IF** \( x_2(t) \) **is** \( M_{i_2} \)

**THEN** \( \dot{x}_m(t) = (A_2 + \Delta A)x_m(t) + (B_2 + \Delta B)x_m(t - h(t)) + E \cos(t) + u(t) \)

\[ (2) \]

where \( x_m(t) \) is a state vector for driving system, \( M_{i_1} (l = 1, 2, 3 \ldots, q, \ i = 1, 2, 3 \ldots, r) \), \( r \) is the fuzzy rules and \( M_{i_1} \) is the fuzzy set, \( x_i(t) (i = 1, 2, 3 \ldots, r) \) is a prevariable, and in this model it is also a prevariable of coronary artery system, \( A_i \) and \( B_i \) are the given system state matrices, \( E \cos(t) \) is the periodic stimulus as defined by medicine, and \( h(t) \) is a time-varying delay satisfying

\[ 0 \leq h(t) \leq \tau, \]

\[ 0 \leq \dot{h}(t) \leq \mu \leq 1 \]

As described above, the fuzzy response system is described as follows.

**Rule I**

**IF** \( \tilde{x}_1(t) \) **is** \( M_{i_1} \)

**THEN** \( \dot{x}_1(t) = (A_1 + \Delta A)x_m(t) + (B_1 + \Delta B)x_m(t - h(t)) + E \cos(t) + u(t) \)

\[ (5) \]

**Rule II**

**IF** \( \tilde{x}_2(t) \) **is** \( M_{i_2} \)

**THEN** \( \dot{x}_1(t) = (A_1 + \Delta A)x_m(t) + (B_1 + \Delta B)x_m(t - h(t)) + E \cos(t) + u(t) \)

\[ (6) \]

where \( x_i(t) \) is a state vector for response system, \( \tilde{x}_i(t) (i = 1, 2, 3 \ldots, r) \) is a prevariable, and in this model it is also a prevariable of coronary artery system and \( u(t) \) is a fuzzy adaptive PDC controller.

The master-slave system has the same rule number, state matrix, and fuzzy set.

In order to study the generality of the stabilization conditions of coronary artery system, we generalize the number of fuzzy rules and obtain a more representative T-S Fuzzy coronary artery system (TSFCAS) model, which has \( r \) fuzzy rules. The system is described as follows.
The master system of TSFCAS is described as follows: for rule $i$ in $r$ fuzzy rules,

$$\text{IF } x_i(t) \text{ is } M_{li},$$

$$\text{THEN } \dot{x}_m(t) = (A_i + \Delta A)x_m(t) + (B_i + \Delta B)x_m(t - h(t)) + E \cos(t)$$

(8)

the slave system of TSFCAS is described as follows: for rule $i$ in $r$ fuzzy rules:

$$\text{IF } x_i(t) \text{ is } M_{li},$$

$$\text{THEN } \dot{x}_s(t) = (A_i + \Delta A)x_s(t) + (B_i + \Delta B)x_s(t - h(t)) + E \cos(t) + u(t)$$

(9)

In the above model, $r$ is the number of fuzzy rules of the system, regulations:

$$m_i(x_i(t)) = \prod_{l=1}^{M} M_{li}(x_l(t)), \quad \sum_{i=1}^{r} m_i(x_i(t)) \geq 0$$

(10)

$$h_i(x_i(t)) = \frac{m_i(x_i(t))}{\sum_{i=1}^{r} m_i(x_i(t))}, \quad h_i(x_i(t)) \geq 0, \quad \sum_{i=1}^{r} h_i(x_i(t)) = 1$$

(11)

Then the TSFCAS model is expressed as follows. The dynamic equation of the master system (driving system) of TSFCAS is as follows:

$$\dot{x}_m(t) = \sum_{i=1}^{r} h_i(x_{mi}(t)) 
\cdot \left[ (A_i + \Delta A)x_m(t) + (B_i + \Delta B)x_m(t - h(t)) \right] + E \cos(t)$$

(12)

The dynamic equation of the slave system (response system) of TSFCAS is as follows:

$$\dot{x}_s(t) = \sum_{i=1}^{r} h_i(x_{si}(t)) 
\cdot \left[ (A_i + \Delta A)x_s(t) + (B_i + \Delta B)x_s(t - h(t)) \right] + E \cos(t) + u(t)$$

(13)

**Remark 1.** The control objective is to design a controller $u(t)$ for the response system, so that the error closed-loop system is composed of the drive system and the response system is stabilized. This paper uses fuzzy PDC controller.

### 3. Fuzzy PDC Controller Design of TSFCAS

In this section, we design a fuzzy PDC controller $u(t)$. For ease of presentation, definitions,

$$h_i = \sum_{i=1}^{r} h_i(x_{mi}(t)) = \sum_{i=1}^{r} h_i(x_{si}(t))$$

(14)

Define the error function as

$$e(t) = x_m(t) - x_s(t)$$

(15)

According to (10) and (11), the error system is as follows:

$$\dot{e}(t) = \dot{x}_m(t) - \dot{x}_s(t)$$

$$= h_i \left[ (A_i + \Delta A)e(t) + (B_i + \Delta B)e(t - h(t)) \right] - u(t)$$

(16)

For each fuzzy rule of the slave system, the rules of the fuzzy adaptive controller are described as follows:

$$\text{IF } x_{si}(t) \text{ is } M_{li},$$

$$\text{THEN } u(t) = K_i e(t)$$

(17)

where $K_i$ is the gain matrix of the PDC controller [28]. Corresponding to the T-S fuzzy dynamic equation of the system, the fuzzy adaptive controller based on PDC is obtained as follows:

$$u(t) = h_i [K_i e(t)]$$

(18)

The error system of the coronary artery fuzzy closed-loop system is obtained as follows:

$$\dot{e}(t) = \dot{x}_m(t) - \dot{x}_s(t)$$

$$= h_i \left[ (A_i + \Delta A)e(t) + (B_i + \Delta B)e(t - h(t)) \right] - u(t)$$

(19)

**Definition 2.** The uncertainties of the system are described as follows:

$$\Delta A = D_a F_a(t) E_a,$$

$$\Delta B = D_b F_b(t) E_b$$

(20)

where $D_a$, $E_a$, $D_b$, $E_b$ are appropriate dimensional constant matrices, and the unknown matrices $F_a(t)$, $F_b(t)$ satisfy

$$F_a^T(t) F_a(t) \leq I,$$

$$F_b^T(t) F_b(t) \leq I$$

(21)

**Lemma 3** ([27]). For a vector-valued function $x(t) \in \mathbb{R}^n$, and other matrices $H_1, H_2 \in \mathbb{R}^{m \times n}$, $Z \in \mathbb{R}^{2n \times 2n}$, and functional $h(t) \geq 0$, and a symmetric positive definite matrix $X \in \mathbb{R}^{m \times m}$, the following integral inequalities hold:

$$- \int_{t-h}^{t} x^T(s) X \dot{x}(s) ds \leq \xi^T(t) Y \xi(t) + h \xi^T(t) Z \xi(t)$$

(22)
where

\[
Y := \begin{bmatrix} H_1^T + H_1 & -H_1^T + H_2 \\ * & -H_2^T - H_2 \end{bmatrix},
\]

\[
\xi(t) := \begin{bmatrix} x(t) \\ x(t-h) \end{bmatrix},
\]

\[
\begin{bmatrix} X & Y \\ * & Z \end{bmatrix} \succeq 0,
\]

\[
Y = [H_1 \ H_2]
\]

\section*{Lemma 4} ([29]). For the symmetric matrices \( F_i \in \mathbb{R}^{n \times n} \), if there exist real scalars \( \epsilon_i \geq 0 \), \( i = 1, 2, 3, \ldots, p \), such that \( F_0 - \sum_{i=1}^{p} \epsilon_i F_i > 0 \), we can get

\[
\Phi^T F_0 \Phi > 0, \quad \forall \Phi \neq 0 \implies \Phi^T F_0 \Phi \geq 0 \quad (24)
\]

\section*{Lemma 5} ([26]). For a given symmetric positive definite matrix \( \zeta \), in \([n_1, n_2] \rightarrow \mathbb{R}^n \), \( \Phi \) is differentiable function, and we have

\[
\begin{bmatrix}
\Gamma_1 & \Gamma_2 & \Gamma_3 & \Gamma_4 & \Gamma_5 & 0 \\
\ast & \Gamma_3 & \frac{\tau^4}{4} B_i^T W D_a & \frac{\tau^4}{4} B_i^T W D_b & \frac{\tau^4}{4} D_i^T W D_a & \frac{\tau^4}{4} D_i^T W D_b \\
\ast & \ast & -\epsilon_1 I + \frac{\tau^4}{4} D_i^T W D_a & \frac{\tau^4}{4} D_i^T W D_b & 0 & 0 \\
\ast & \ast & \ast & -\epsilon_2 I + \frac{\tau^4}{4} D_i^T W D_b & 0 & 0 \\
\ast & \ast & \ast & \ast & -3W & 6W \\
\ast & \ast & \ast & \ast & \ast & \frac{18}{\tau^2} W \\
\ast & \ast & \ast & \ast & \ast & -V \\
\ast & \ast & \ast & \ast & \ast & -V \\
\end{bmatrix} < 0, \quad (27)
\]

where

\[
\Gamma_1 = PA_1 + A_1^T P + PK_1 + K_1^T P + Q + H_1 + H_1^T + \epsilon_1 E_1^T E_1 + \frac{\tau^4}{4} A_1^T W A_1 - \frac{\tau^4}{4} A_1^T W K_i - \frac{\tau^4}{4} K_i^T W A_1 - \frac{\tau^4}{4} K_i^T W K_i - \left(1 - \frac{3}{2}\right) \frac{\tau^4}{4} W - A_1^T V K_i - K_1^T V A_1 - K_1^T V K_i
\]

\[
\Gamma_2 = PB_1 - H_1^T + H_2 + \frac{\tau^4}{4} A_1^T W B_1 - \frac{\tau^4}{4} K_i^T W B_1 - K_1^T V B_i
\]

\section*{4. Main Result}

In this section, we use the lemma mentioned above to get a new synchronization method.

\section*{Theorem 6.} Consider coronary artery fuzzy closed-loop error system, for a given constant \( \tau > 0 \), \( \epsilon_1 \geq 0 \), \( \epsilon_2 \geq 0 \), if there exist positive symmetric matrices \( P > 0 \), \( Q > 0 \), \( V > 0 \), \( W > 0 \), and any matrices \( H_1, H_2 \), satisfying the following LMI:

\[
\int_{n_1}^{n_2} \int_{\theta}^{n_1} \Phi^T(t) \Phi(t) d\theta d\theta \leq \eta_1^T \zeta \eta_1 + 2\eta_2^T \zeta \eta_2 \quad (25)
\]

\[
\text{where}
\]

\[
\eta_1 = \frac{2}{(n_2 - n_1)} \Phi (n_2) - \frac{2}{(n_2 - n_1)^2} \int_{n_1}^{n_2} \Phi (\theta) d\theta
\]

\[
\eta_2 = \frac{1}{(n_2 - n_1)} \Phi (n_2) - \frac{2}{(n_2 - n_1)^2} \int_{n_1}^{n_2} \Phi (\theta) d\theta + \frac{6}{(n_2 - n_1)^3} \int_{n_1}^{n_2} \int_{\theta}^{n_1} \Phi (t) d\theta d\theta
\]

Then the closed-loop coronary artery error system will be asymptotically stable.

\section*{Proof.} Construct the following LKF:

\[
V(t) = \sum_{i=1}^{m} V_i(t), \quad (29)
\]
where

\[
V_1(t) = e^T(t) Pe(t), \quad (30)
\]
\[
V_2(t) = \int_{t-h(t)}^t e^T(s) Qe(s) ds, \quad (31)
\]
\[
V_3(t) = \int^0_{t-\tau} \int_{t-\tau}^t \bar{e}^T(s) R \bar{e}(s) ds \, d\theta, \quad (32)
\]
\[
V_4(t) = \frac{\tau^2}{2} \int_{t-\tau}^t \int_s^t \bar{e}^T(v) \dot{W}(v) dv \, du \, ds, \quad (33)
\]

The time derivative of \( V(t) \)

\[
\dot{V}(t) = \sum_{i=1}^{4} \dot{V}_i(t), \quad (34)
\]

where

\[
\dot{V}_1(t) = \dot{e}^T(t) Pe(t) + \dot{e}^T(t) Pe(t) = h_1 [\dot{e}^T(t) \cdot P (A_i + \Delta A - K_i) + (A_i + \Delta A - K_i)^T P] e(t) \]
\[
+ h_1 \left[ 2\dot{e}^T(t) P (B_i + \Delta B) e(t-h(t)) \right] \]
\[
\dot{V}_2(t) = h_1 \left[ \dot{e}^T(t) Qe(t) \right] - h_1 \left[ (1-\mu) \dot{e}^T(t-h(t)) \cdot Qe(t-h(t)) \right] \]
\[
\dot{V}_3(t) = \tau \dot{e}^T(t) R \dot{e}(t) - \int_{t-\tau}^t \dot{e}^T(s) R \dot{e}(s) ds \]
\[
\dot{V}_4(t) = \frac{\tau^4}{4} \dot{e}^T(t) \dot{W}(t) - \frac{\tau^2}{2} \int_{t-\tau}^t \int_s^t \dot{e}^T(u) \dot{W}(u) du \, ds \]

For \( \dot{V}_5(t) \), according to Lemma 3, we obtain

\[
\dot{V}_5(t) = \tau \dot{e}^T(t) R \dot{e}(t) - \int_{t-\tau}^t \dot{e}^T(s) R \dot{e}(s) ds \leq \tau \dot{e}^T(t) R \dot{e}(t) - \int_{t-\tau}^t \dot{e}^T(s) R \dot{e}(s) ds \]
\[
\leq \tau \dot{e}^T(t) R \dot{e}(t) + h_1 \left[ \dot{\xi}^T(t) \Xi \dot{\xi}(t) + \tau \dot{\xi}^T(t) Z \dot{\xi}(t) \right] \]

where

\[
\psi(t) = \begin{bmatrix} e^T(t) & e^T(t-h(t)) & (F_a(t) E_a e(t))^T & (F_b(t) E_b e(t-h(t)))^T & \int_{t-\tau}^t e^T(s) ds \int_{t-\tau}^t e^T(u) du \end{bmatrix}^T \]
\[
\Xi = \begin{bmatrix} \Lambda_1 & \Lambda_2 & \Lambda_4 & \Lambda_5 & 0 & 3W \end{bmatrix}
\]

\[
= \begin{bmatrix} \Lambda_1 & \Lambda_2 & \Lambda_4 & \Lambda_5 & 0 & 3W \\
* & \Lambda_3 & \tau B_i^T R D_a + \frac{\tau^4}{4} B_i^T W D_a & \tau B_i^T R D_b + \frac{\tau^4}{4} B_i^T W D_b & 0 & 0 \\
* & * & \tau D_i^T R D_a + \frac{\tau^4}{4} D_i^T W D_a & \tau D_i^T R D_b + \frac{\tau^4}{4} D_i^T W D_b & 0 & 0 \\
* & * & * & \tau D_i^T R D_b + \frac{\tau^4}{4} D_i^T W D_b & 0 & 0 \\
* & * & * & * & -3W & \frac{8}{3} W \\
* & * & * & * & * & -\frac{18}{\tau^2} W \end{bmatrix} < 0, \quad (44)
\]

For \( \dot{V}_4(t) \), the proposed Lemma 5 was applied as follows:

\[
\frac{\tau^2}{2} \eta(t) \geq \phi_1^T(t) W \phi_1(t) + 2\phi_2^T(t) W \phi_2(t) \quad (41)
\]

where

\[
\eta(t) = \int_{t-\tau}^t \int_{s} e^T(u) \dot{W}(u) du \, ds \]
\[
\phi_1(t) = \int_{t-\tau}^t \int_{s} \dot{e}(u) du \, ds = \dot{h}(t) - \int_{s} e(s) ds \]
\[
\phi_2(t) = \int_{t-\tau}^t \int_{s} \dot{e}(u) du \, ds \quad (42)
\]

Combining (27), (29), (32), and (33), we obtain

\[
\dot{V}(t) \leq h_1 \psi^T(t) \Xi \psi(t) \quad (43)
\]
where
\[
\Lambda_1 = PA_1 + A_1^T P + PK_i + K_i^T P + Q + H_i + H_i^T
\]
\[+ \tau A_1^T R A_1 + \tau H_i^T R^{-1} H_i + \frac{\tau^4}{4} A_1^T W A_1
\]
\[- \frac{\tau^4}{4} A_1^T W K_i - \frac{\tau^4}{4} K_i^T W A_1 + \frac{\tau^4}{4} K_i^T W K_i
\]
\[- \frac{3}{2} \tau^2 W - \tau A_i^T R K_i - \tau K_i^T R A_i + \tau K_i^T R K_i
\]
\[
\Lambda_2 = PB_i - H_i^T + H_2 + \tau A_i^T R B_i + \tau H_i R^{-1} H_2
\]
\[+ \frac{\tau^4}{4} A_i^T W B_i - \frac{\tau^4}{4} K_i^T W B_i - \tau K_i^T R B_i
\]
\[
\Lambda_3 = \tau B_i R B_i - (1 - \mu) Q - H_2^T + H_2 + \tau H_2 R^{-1} H_2
\]
\[+ \frac{\tau^4}{4} R^T W B_i
\]
\[
\Lambda_4 = PD_a + \tau A_i^T R D_a + \frac{\tau^4}{4} A_i^T W D_a - \frac{\tau^4}{4} K_i^T W D_a
\]
\[- \tau K_i^T R D_a
\]
\[
\Lambda_5 = PD_b + \tau A_i^T R D_b + \frac{\tau^4}{4} A_i^T W D_b - \frac{\tau^4}{4} K_i^T W D_b
\]
\[- \tau K_i^T R D_b
\]

If \( \Xi < 0 \), we obtain \( \hat{V}(t) < 0 \). Applying condition (5), we have that
\[
(F_a(t) \dot{e}_a(t))^T (F_a(t) \dot{e}_a(t)) \leq e_a^T(t) E_a^T E_a e(t) \tag{46}
\]
and similarly we can get
\[
(F_b(t) \dot{e}_b(t - h(t)))^T (F_b(t) \dot{e}_b(t - h(t))) \leq e_b^T(t - h(t)) E_b^T E_b e(t - h(t)) \tag{47}
\]
and by using Lemma 4, we can define
\[
\epsilon_1 \geq 0,
\]
\[
\epsilon_2 \geq 0,
\]
\[
T_1 = \text{diag} \left[ E_a^T E_a \ 0 \ -I \ 0 \ 0 \ 0 \right],
\]
\[
T_2 = \text{diag} \left[ 0 \ E_b^T E_b \ -I \ 0 \ 0 \ 0 \right]
\]
such that \( \Xi + \epsilon_1 T_1 + \epsilon_2 T_2 < 0 \). Considering the existence of nonlinear terms such as \( \tau A_i^T R A_i \), in inequalities, definition \( V = \tau R \), applying the well-known Schur complement, we can get LMI (18). This completes the proof. \( \square \)

Remark 7. Systems (12) and (13) are asymptotically synchronized if the error system (15) satisfies
\[
t \rightarrow \infty, \ e(t) \rightarrow 0.
\]
In this paper, we design LKF (29) and can get the LMI (27) is less than zero by using the MATLAB LMI toolbox, achieving asymptotic stability of the error closed-loop system (15).

Remark 8. Compared with the traditional system model to the problem of tracking control behavior, T-S fuzzy chaotic system model used IF-THEN fuzzy rules to represent the local dynamic characteristics of chaotic systems. The latter part of each fuzzy rule is represented by the linear model of the local region of the state space, and the T-S fuzzy model of the nonlinear system is obtained by the integration of the local models. The controller based on T-S fuzzy model can be designed by using the linear system control theory and Lyapunov theory. This is the advantage of using T-S fuzzy chaotic system model in this paper.

5. Simulation

In this section, we will give the following numerical examples to demonstrate the effectiveness of the proposed control strategy.

Example 1. According to the follow parameters, we can get the phase portraits of TSFCAS (12), (13).

\[
A_1 = \begin{bmatrix}
-0.15 & 1.7 \\
-49.425 & -0.35
\end{bmatrix},
\]
\[
A_2 = \begin{bmatrix}
-0.15 & 1.7 \\
0.575 & -0.35
\end{bmatrix},
\]
\[
B_1 = \begin{bmatrix}
0 & 0 \\
0.01 & 0.01
\end{bmatrix},
\]
\[
B_2 = \begin{bmatrix}
0 & 0 \\
0.01 & 0.01
\end{bmatrix},
\]
\[
D_1 = E_1 = \begin{bmatrix}
\sqrt{1.6} & 0 \\
0 & \sqrt{0.05}
\end{bmatrix},
\]
\[
D_2 = E_2 = \begin{bmatrix}
\sqrt{0.1} & 0 \\
0 & \sqrt{0.3}
\end{bmatrix},
\]
\[
F_a(t) = F_b(t) = \begin{bmatrix}
0.5 \sin(t) & -0.5 \cos(t) \\
-0.5 \cos(t) & 0.5 \sin(t)
\end{bmatrix}
\]

The membership functions of the TSFCAS (12), (13) are selected as
\[
h_1(x_{m1}(t)) = 1 - \frac{x_{m1}^2}{h^2},
\]
\[
h_2(x_{m2}(t)) = \frac{x_{m2}^2}{h^2} \quad \text{for} \quad h^2 = 100
\]
Complexity

\[ h_1(x_1(t)) = 1 - \frac{x_1^2}{h^2}, \]

\[ h_2(x_2(t)) = \frac{x_2^2}{h^2} \]  \hspace{1cm} (51)

Initial conditions of the TSFCAS (12), (13) are selected as \( x_m(0) = (0.2, 0)^T \), \( x_i(0) = (-0.1, 0.2)^T \), and we choose the time-varying delay as \( h(t) = 0.125 \sin(2t) \). On the basis of LMI (27), we can gain matrices \( P, Q, W \) by using MATLAB LMI toolbox, and we can obtain the gain matrices \( K_1, K_2 \) in controller (18) by using MATLAB LMI toolbox.

\[ P = \begin{bmatrix} 97.9946 & 0.0000 \\ 0.0000 & 97.9946 \end{bmatrix}, \]

\[ Q = \begin{bmatrix} 114.8543 & 0.00704 \\ 0.0070 & 120.8465 \end{bmatrix}, \]

\[ W = \begin{bmatrix} 2.4879 & -0.0005 \\ -0.0005 & 2.6188 \end{bmatrix}, \]  \hspace{1cm} (52)

\[ K_1 = \begin{bmatrix} -0.2473 & -0.0194 \\ -0.0224 & 0.4494 \end{bmatrix}, \]

\[ K_2 = \begin{bmatrix} 1.1317 & 0.3703 \\ 0.2518 & 0.4494 \end{bmatrix}. \]

The membership functions and initial conditions of the TSFCAS (12), (13) and the time-varying delay \( h(t) \) are the same as Example 1. On the basis of LMI (27), we can gain matrices \( P, Q, W \) by using MATLAB LMI toolbox, and we can obtain the gain matrices \( K_1, K_2 \) in controller (18) by using MATLAB LMI toolbox.

\[ A_1 = \begin{bmatrix} -0.1 & 2.2 \\ -30.575 & -0.3 \end{bmatrix}, \]

\[ A_2 = \begin{bmatrix} -0.1 & 2.2 \\ 0.575 & -0.35 \end{bmatrix}, \]

\[ B_1 = \begin{bmatrix} 0 & 0 \\ 0.02 & 0.02 \end{bmatrix}, \]

\[ B_2 = \begin{bmatrix} 0 & 0 \\ 0.02 & 0.02 \end{bmatrix}, \]  \hspace{1cm} (53)

\[ D_1 = E_1 = \begin{bmatrix} \sqrt{1.8} & 0 \\ 0 & \sqrt{0.05} \end{bmatrix}, \]

\[ D_2 = E_2 = \begin{bmatrix} \sqrt{0.3} & 0 \\ 0 & \sqrt{0.2} \end{bmatrix}, \]

\[ F_a(t) = F_b(t) = \begin{bmatrix} 0.5 \sin(t) & -0.5 \cos(t) \\ -0.5 \cos(t) & 0.5 \sin(t) \end{bmatrix}. \]

where Figures 1(a) and 2(a) show the phase diagram of coronary drive chaotic system, which can observe that CAS showed obvious chaotic behavior. Figure 1(b) shows the phase diagram of coronary response chaotic system without controller \( u(t) \) and Figure 2(b) shows the phase diagram of coronary response chaotic system with controller \( u(t) \). With controller \( u(t) \), we can see that the trajectory of coronary response chaotic system (Figure 2(b)) synchronization of the trajectory of coronary drive chaotic system Figure 1(a).

The error plots between systems (12) and (13) with different initial conditions and without controller \( u(t) \) can be shown.

\[ K_1 = \begin{bmatrix} -0.2779 & -0.0541 \\ -0.0455 & 0.1406 \end{bmatrix}, \]

\[ K_2 = \begin{bmatrix} 1.1854 & 0.4122 \\ 0.3389 & 0.1344 \end{bmatrix} \]  \hspace{1cm} (54)

where Figures 3(a) and Figure 3(b) show the phase diagram of coronary drive chaotic system, which can observe that CAS showed obvious chaotic behavior. Figure 1(b) shows the phase diagram of coronary response chaotic system without controller \( u(t) \) and Figure 4(b) shows the phase diagram of coronary response chaotic system with controller \( u(t) \). With controller \( u(t) \), we can see the trajectory of coronary response chaotic system (Figure 4(b)) synchronization of the trajectory of coronary drive chaotic system Figure 1(a). The error plots between systems (12) and (13) with different initial conditions and without controller \( u(t) \) can be shown.
in Figure 3(c). Figure 4(d) plots the input of fuzzy PDC controller. Through the PDC controller of fuzzy model \( u_1(t) \) and \( u_2(t) \) (Figure 4(d)), we can see that the error plots between systems (12) and (13) tend to zero in Figure 4(c). The simulation result indicated, this paper proposed the method is correct and effective and has certain practical significance. When given different scaling factor, we can see the difference between Examples 1 and 2, such that comparing the error plots between systems (12) and (13) tends to zero time; we can see Figure 2(c) is faster than Figure 4(c), and control signal \( u(t) \) control time in Figure 4(c) also needs a little longer.

In the biological and medical sense, by using a synchronization controller to synchronize the chaotic motion state of the diseased vessels to that of the normal vessels, so as to achieve the goal of treatment, it can be seen that the study of coronary vascular chaos synchronization helps to better prevent and treat myocardial infarction, angina pectoris, and other diseases that seriously endanger human health. The CAS is actually a complex nonlinear system and is subject to interference by external factors. For such complex nonlinear systems with uncertain parameters, the T-S fuzzy model can be considered for more precise description. The T-S fuzzy model can well realize the linearization of nonlinear systems and can play an effective role in controller design. Using the T-S fuzzy model, a chaotic system can be regarded as the weighted sum of multiple local linear models, and then the parallel distributed compensation method is used to design the controller,
Figure 2: Behavior of the master-slave systems with control signal.

Figure 3: Behavior of the master-slave systems without control signal.
thus effectively solving the chaotic synchronization control problem.

6. Conclusions

This paper has studied based on the T-S fuzzy model indefinite coronary artery system chaos synchronization control issue. By constructing the uncertain dynamic equation of the coronary artery system, a PDC controller whose fuzzy rule corresponds to the fuzzy model is designed. By using Wirtinger-based double inequality and an improved Moon et al.’s inequality to construct the appropriate Lyapunov functional, the conditions for system stability in LMI form are derived. Simulation results show that the method proposed in this paper is correct and effective and has certain practical significance. The stability criterion proposed in this paper reduces the conservativeness to a certain extent, but there is still a lot of space for improvement. In the study of CAS, the system is frequently complex and uncertain. Due to the fact that the membership degree of traditional fuzzy sets is two-dimensional, it is very difficult to describe that different objects belong to different fuzzy sets, especially for highly uncertain systems, to improve the system’s ability to handle uncertainty. While the membership functions of type-2 fuzzy sets are three-dimensional, it provides the extra degree of freedom the third dimension. In highly uncertain systems, type-2 fuzzy sets are always better than traditional fuzzy sets. Therefore, the application of type-2 fuzzy model to more complex CAS will be an important research topic in the future.
Data Availability

The data used to support the findings of this study are available from the corresponding author upon request.

Conflicts of Interest

The authors declare that they have no conflicts of interest.

Acknowledgments

This work is supported in part by the Natural Science Foundation of Tianjin City (18JCJB08100 and 15JCJB16100) and the Natural Science Foundation of China (61503280).

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