Calibration and standardisation of synchrotron radiation and conventional circular dichroism spectrometers. Part 2: Factors affecting magnitude and wavelength

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Abstract. Circular dichroism (CD) spectroscopy is an important tool in structural biology, especially for protein secondary structure analyses. Synchrotron radiation circular dichroism (SRCD) spectroscopy is a modified version of the technique that uses the intense light from a synchrotron source to enable the collection of data to much lower wavelengths than possible on conventional circular dichroism (cCD) instruments. There is a need for standardization of calibration methods amongst and between cCD and SRCD instruments to ensure consistency and the ability to use common reference databases for empirical secondary structural analyses. In a previous study (*Spectroscopy* **17** (2003), 653–661), we compared optical rotation measurements on several cCD and SRCD instruments, whilst holding constant other experimental factors. In this study, other experimental parameters which contribute to the spectral magnitude, such as cell pathlength and protein concentration determinations, are examined. In addition, the extent of wavelength calibration variations between instruments and their effects on secondary structure calculations have been examined. Hence, this paper provides additional practical guidance for “good practice” in the measurement of CD data.

1. Introduction

Circular dichroism (CD) spectroscopy is a long-established technique for examining the secondary structure of proteins and for monitoring protein interactions and folding pathways. It is gaining acceptance as a technique approved for the characterization of macromolecules for pharmacological use. Synchrotron radiation-based circular dichroism (SRCD) spectroscopy made its debut more than 20 years ago [1,2], but its full potential for the study of protein structures has only recently been exploited. The intense light from the synchrotron source permits the collection of higher quality data than that obtained using conventional circular dichroism (cCD) instruments and appreciably extends the lower wavelength limit of the data [3]. It has been suggested that the extra information available in the vacuum ultraviolet (VUV) data will allow more accurate discernment of structural features, potentially even including information on folds and motifs [4]. To this end, new reference databases of circular dichroism spectra which include the lower wavelength data and a wider base of protein structural types, are being created

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[4,5] to enable improved analyses. For these to be useful with both cCD and SRCD data, it is necessary to establish a consistent set of calibration standards and protocols to ensure compatibility between and amongst SRCD and cCD instruments.

In a previous study [6], the optical rotation magnitude measurements for a number of standard compounds plus one protein were measured on several SRCD and cCD instruments, whilst holding other potential variables (sample, sample cell, measurement parameters, instrument operator, etc.) constant in order to strictly examine the extent of variation between instruments. Based on this, a method was proposed for the standardisation of protein spectra, to “correct” for the instrumental variations [6,7].

However, in addition to instrumental variations, errors in spectral magnitude arising from other sources can produce serious errors in protein secondary structures calculated from CD data [8]. Potential sources of magnitude error that were not tested in the previous study because the same sample in the same cell was used for all measurements, are the determinations of protein concentration and cell pathlength. In the present study two popular methods for measuring protein concentration, the A_{280} in the presence of denaturant [9] and quantitative amino acid analysis (QAA) are compared. In addition, two methods for measuring cell pathlengths, the interference fringe method [10] and the chromate dilution method are compared.

Another source of instrumental error can arise from misalignment or miscalibration of the instrument monochromator, which can lead to apparent shifts of wavelength that are manifest as differences in peak positions. These, too, will have a significant effect on empirical analyses of protein spectra. In this study we not only show the effects of wavelength shifts on the analyses of secondary structure, but also examine simple means of accurately calibrating instruments to eliminate this source of error. If an instrument spectral resolution of at least 0.2 nm could be achieved, benzene vapour was used as it produces a series of sharp peaks between 270 nm and 230 nm [11]. In addition, a certified holmium oxide filter was used to measure the wavelength variations in the near UV and visible regions; the results obtained by these two methods were compared.

In summary, this paper reports on a number of practical issues that can affect measurements of cCD and SRCD spectra, and describes means of accurately determining parameters which contribute to spectral magnitude, such as protein concentration and cell pathlength.

2. Materials and methods

2.1. Materials

Horse skeletal myoglobin was purchased from ICN Biochemicals, chicken lysozyme from Worthington, human serum ceruloplasmin from Calbiochem (USA). Human serum albumin (HSA), jackbean concanavalin A (Con A), and chicken avidin were from Sigma-Aldrich Company Ltd. All proteins had a purity of >95%. Prior to use, each sample was dialysed, centrifuged and degassed as described in Miles et al. [6].

Benzene (AnalaR grade) was obtained from BDH Laboratory supplies, UK. (+)-Camphor-10-sulfonic acid, 99% purity, guanidine hydrochloride, >99% purity, and potassium chromate (K_2CrO_4), 99.99% purity, were obtained from Sigma-Aldrich Company Ltd. A certified holmium oxide glass filter from Hellma UK Ltd. was used.

2.2. CD and SRCD spectroscopic measurements

cCD measurements were made on an Aviv 62Ds, an Aviv 215, a JASCO 600 and a JASCO 715 instrument. SRCD measurements were made at the SRS Daresbury (UK) on beamline CD12; at ISA (Den-

mark) on beamline UV1; at the NSLS (USA) on beamlines U9b and U11; and at BESSY2 (Germany) on beamline 3m_NIM1_C.

The holmium oxide glass filter was scanned from 600 to 200 nm on the cCD instruments but only from 400 to 200 nm on the SRCD instruments, due to limitations in their high wavelength ranges. Other parameters used were: bandwidth 1 nm, step size 0.1 nm, averaging/dwell time 0.2 sec and temperature 25°C. The benzene sample was prepared by introducing one drop of benzene into a 1 cm cuvette, which was then tightly stoppered. The high tension (HT) or dynode signal of the vapour was recorded over the wavelength range from 270 to 240 nm with a step size of 0.1 nm, an averaging/dwell time of 0.2 sec and at temperature of 25°C. The bandwidth was set to 0.1 nm on three cCD instruments and on UV1, at 0.2 nm (the lowest possible). The narrowest possible bandwidth was used on 3m_NIM1_C, which had no calibrated bandwidth control at the time. CD12, U96 and U11 did not allow resolutions of lower than 0.5 nm therefore the sharp benzene peaks could not be measured on them accurately. The protein spectra and baselines were collected using the same (nominally) 0.001 cm pathlength circular demountable cell (Hellma UK Ltd.) over the wavelength range from 280 to 178 nm on conventional instruments and over the range from 280 to 168 nm on SRCD machines. On all instruments the bandwidth was set at 1 nm, step size 0.2 nm, averaging/dwell time 1 s, and temperature 4°C. An average of 3 scans was used in each case.

2.3. Secondary structure calculations

The secondary structural analyses used the DICHROWEB <http://www.cryst.bbk.ac.uk/cdweb> interactive webserver [12] with the CONTINLL [13] algorithm and database 1 [14].

2.4. Sample cell pathlength determinations

A UV/VIS spectrophotometer (CARY 3) was used in transmission mode, with a step size of 0.2 nm, bandwidth of 1 nm, and an air baseline collected between 650 and 350 nm, followed by a scan of the empty cell. The pathlengths of a number of cells were determined according to the formula given in the legend for Fig. 1.

Fig. 1. Interference fringes obtained by scanning an empty sample cell with a nominally 0.001 cm pathlength using an UV/VIS spectrophotometer in transmission mode. The cell pathlength, calculated from the formula $PL(\mu m) = [(n(W1 * W2))/(2(W2 - W1))]/1000$, where $W1$ and $W2$ are the wavelengths of the first and last fringes in nm and n is the number of fringes between the $W1$ and $W2$.

For the chromate dilution method, 1 litre of 0.02 M potassium chromate in 0.01 M NaOH was prepared gravimetrically. 0.002 M and 0.0002 M solutions were prepared by serial dilution. Pathlengths were determined using $\epsilon_{372} = 4830 \text{ mol l}^{-1} \text{ cm}^{-1}$ [15].

2.5. Protein concentration determinations

For each sample, the protein concentration was measured using the absorbance method of Gill and von Hippel [9] in the presence of guanidine hydrochloride. In addition, two separate 10 μl aliquots of each protein sample were examined by quantitative amino acid analysis (QAA) at the PNAC facility, University of Cambridge.

3. Results

3.1. Sample cell pathlength determinations

To achieve the full potential of SRCD instruments to measure low wavelength data, it is necessary to use short demountable pathlength cells ($\leq 0.005 \text{ cm}$) to minimize the absorption due to water, buffer, and salts. Whilst the pathlengths of long cells (0.1–1.0 cm) are usually accurately reported by the manufacturers, the reported pathlengths of short cells can be in error by as much as 50%, which in turn will result in this level of error in the spectral magnitudes. Accurate measurement of the cell pathlength can be achieved by using the interference fringe method [10]. This relies on a portion of the incident beam being retarded by double reflection from the inner surfaces of the empty cell. An interference pattern is produced in the visible and UV transmission spectrum (Fig. 1) when the retarded beam interferes with the main beam and the distance between the peaks is inversely proportional to twice the cell pathlength. When measuring the cell pathlength, the cell must be loaded into the same cell holder used when measuring the CD spectrum with the two halves of the cell in the same orientation relative to each other to achieve reproducible results. It should be noted that this method gives a minimum pathlength for a demountable cell since a thin layer of liquid can form between the flanges when a sample is added, increasing the pathlength by 0.5–1 μm , although this can be avoided by careful loading with the smallest possible sample volume so it does not overflow into the spacer region, or by designing cells with a different loading geometry (Wien and Wallace, in preparation). In this study the pathlengths of a number of nominally 10 μm quartz Suprasil cells were found to range from 12 to 16 μm , while cells reported as being $4 \pm 1 \mu\text{m}$ were found to be between 6 and 7 μm . In the latter case this is a 75% error. Very similar results were obtained using the potassium chromate dilution method, with the results deviating from the fringe results by only 2–3%. However, for very short pathlength cells, the interference fringe method is more accurate as it is not dependent on precise measurements of small absorbances.

3.2. Protein concentration determinations

The concentrations of a number of proteins were measured both by using their absorbance at 280 nm (in 6 M guanidine hydrochloride) and by quantitative amino acid analysis (Table 1). For the QAA measurements, two aliquots of each protein sample were examined, and in the worse cases there was a difference of $\sim 5\%$ between the two values obtained by QAA, although the variance was often as low as 1%. The differences between the two methods were compared, and were found, in all but one case, to be larger than the deviations in the QAA measurements. In addition, in all cases except that one, the A_{280} -determined value was larger than the QAA value.

Table 1

Comparison of the results of protein concentration determinations by the methods of Gill and von Hippel (GvH) [19] and duplicate quantitative amino acid analyses (QAA)

Protein	Concentration by $A_{280\text{nm}}$	QAA average	QAA SD	Difference $ QAA - GvH $
Con A	10.7	9.69	0.08	1.01
Lysozyme	9.4	8.54	0.45	0.86
Myoglobin	7.4	7.46	0.44	0.06
Avidin	12.3	10.01	0.04	2.29
HSA	5.5	5.22	0.24	0.28
Ceruloplasmin	11.4	10.16	0.10	1.12

Note that where the difference between the values obtained by the different methods is less than the standard deviation (SD) of the measurements, the value is in bold italics.

Table 2

Wavelength calibrations showing the peak positions (in nm), as measured on different instruments for benzene vapour and a certified holmium oxide filter compared with literature values. The peak position of the positive $\pi \rightarrow \pi^*$ exciton peak of the protein myoglobin (Mb) is also included for comparison. Values for cCD1 are shown before (init) and after (recal) recalibration

	Literature value	cCD1		cCD2	cCD3	cCD4	SRCD1	SRCD2	SRCD3	SRCD4	SRCD5
		init	recal								
Benzene vapour	241.7	240.1	241.6	241.8	241.6	241.8	–	241.7	242.7	–	–
	253.0	252.0	252.8	253.1	252.9	253.1	–	253.0	253.7	–	–
	260.1	259.1	259.8	260.1	260.0	260.0	–	260.0	260.8	–	–
Holmium oxide filter	279.2	278.1	279.1	279.2	279.0	280.0	279.1	279.3	–	280.6	279.1
	360.9	359.4	360.3	361.6	361.0	362.0	360.7	–	–	362.3	–
	453.7	451.7	452.5	454.0	454.0	455.0	–	–	–	–	–
Myoglobin		191.6	192.3	192.2	192.0	192.6	192.0	192.2	193.0	193.1	192.0

3.3. Wavelength comparisons

The holmium glass filter produces peaks at 279.2 nm, 360.9 nm, and 453.65 nm. However most existing SRCD detectors are limited to wavelengths below 350 nm; consequently, only the 279.2 nm peak could be measured on these instruments. In the UV range, for three of the SRCD instruments the holmium oxide filter gave rise to peaks within 0.1 nm of the certified wavelength (Table 2). On one conventional instrument this peak was shifted by +0.8 nm while the other cCD instruments were accurate to within 0.2 nm, which is well within instrument specifications. These variances are roughly comparable to the wavelength shifts seen for the 260.1 nm, 253.0 nm and 241.7 nm benzene peaks. One SRCD instrument for which no holmium oxide measurement could be obtained, exhibited shifts ranging between +1.0 and +0.7 nm for the benzene peaks. The results are shown in Fig. 2 as a plot of expected versus measured wavelength. In the UV range the biggest difference (after re-calibration) was 1.0 nm. However, the wavelength shifts increased in the visible range to deviations from the literature value of as much as 1.3 nm on one instrument and a net difference between instruments of 2.5 nm. Very similar trends were seen for the benzene and holmium standards. Benzene has an advantage of having several measurable peaks in the UV region where most protein peaks are, but it has the disadvantage of requiring the ability to set a small bandwidth for the measurement of its sharp peaks.

Fig. 2. Plot of expected (literature values) versus measured wavelength positions (in nm) showing variations between different instruments in the absorption peaks of a certified holmium oxide glass filter and benzene vapour. The open symbols correspond to conventional CD instruments, the filled symbols to SRCD instruments.

Table 3
Effect of (artificial) wavelength shifts on calculated secondary structure contents for several proteins

Protein	Wavelength shift (nm) applied	Calculated helix content (%)	Calculated sheet content (%)
Myoglobin	0	75	0
	+1	77	0
	-1	69	1
HSA	0	72	1
	+1	72	2
	-1	70	1
Lysozyme	0	38	14
	+1	39	15
	-1	36	13
Con A	0	9	39
	+1	7	42
	-1	11	37
Avidin	0	1	53
	+1	1	52
	-1	1	51
Ceruleplasmin	0	3	33
	+1	4	34
	-1	4	32

The wavelength variations seen in the standards are also reflected in the spectra measured for myoglobin on these instruments where the difference in the measured position of the positive $\pi \rightarrow \pi^*$ exciton peak at ~ 192 nm is as much as 1.1 nm on different instruments. To illustrate the effect of this type of wavelength shift on secondary structure analyses (without other factors such as optical rotation magnitude contributing to the difference) the CD spectra of a number of proteins were artificially shifted by +1 nm and -1 nm and the calculated secondary structures from the resulting spectra were compared.

Table 3 shows that wavelength shifts can have a small but significant effect on the calculated helix and sheet content of proteins. For example a shift of +1 nm leads to a small increase in the predicted helix content in the mostly helical protein myoglobin (from 75% to 77%), while a shift of -1 nm causes a decrease to 69%. It appears generally (but not always) that for the mostly helical proteins (myoglobin, HSA and lysozyme) shifts of +1 nm tend to increase calculated helical content and decrease sheet content; the converse results are true for shifts of -1. The effects on the mostly sheet proteins are less pronounced, but often +1 shifts lead to increased sheet contents and -1 shifts lead to decreased sheet contents. The effects of errors in peak positions are not nearly as dramatic as those produced by errors in spectral magnitude [8], nevertheless, they have discernable consequences on the calculated structures.

4. Conclusion

A major potential source of magnitude error, incorrect cell pathlength, is more commonly found for short pathlength cells. If a 1 mm cell deviates by 10 μm , this only gives rise to an error of 1%; however if a 10 μm cell deviates by 4 μm , as was found in this study, this results in a 40% error, which is unacceptable for quantitative experiments. For pathlengths between 50 μm and 1 mm, carefully prepared solutions of potassium chromate can be used for calibration. But for very short pathlength cells, the absorbance values are too small for accurate determinations. For these cells the interference fringe method gives a more precise measurement, with an error of $\leq 0.2 \mu\text{m}$. This method cannot, however, be used for cells with pathlengths longer than $\sim 20 \mu\text{m}$ for practical reasons, based on the number of resolvable fringes.

Similarly, it is essential to have accurate values for protein concentrations. The best, although most costly, results are obtained by quantitative amino acid analysis. This method requires only small amounts of sample ($\sim 1 \text{ nmole}$) and involves the hydrolysis of the protein into its constituent residues, which are then derivitised for detection by fluorescence and separated by column chromatography. If the sequence of the protein is known, then the quantitation of well-recovered residues, mainly those with small hydrophobic side chains, in the presence of a standard, provides an accurate measure at the concentration of the protein. If the sequence is not accurately known, there are alternative methods of recovering all residues including the most labile ones such as tryptophan [16]. In a comparison of absorbance methods versus QAA for bovine serum albumin, it was found that other methods including the use of $A_{280 \text{ nm}}$ tended to overestimate the concentration of the protein, probably due to undetected bound salts and water molecules [17], a trend which was also seen for the other proteins examined in the present study (Table 2). Absorption methods can also be affected by pH, temperature, buffer composition and light scattering, not accounted for in the standard empirical calculation methods. Obviously gravimetric methods, which are often relied on instead, can also be severely affected by other components present such as salts, buffers, etc., which contribute to the apparent amount weighed out, and are subject to even larger errors.

The effect of monochromator misalignment may appear small when visually comparing spectra but wavelength shifts of as little as 1 nm can have a significant effect on secondary structure analyses. It should be noted that an apparent shift in wavelength can also result from setting the spectra acquisition time constant too low or having a protein concentration that is too high [8]. It is necessary to check the calibration of an instrument at several wavelengths including at least one in the far UV where the protein amide absorption occurs. Benzene vapour, which is usually used to determine the wavelength resolution of an instrument, provides a cheap method to calibrate wavelength. Although the useful range is small,

between 240 and 270 nm the peaks are much sharper than those of the holmium oxide glass filter, which are at higher wavelengths.

Acetone vapour has been suggested as an alternative wavelength standard for the far UV, as it gives rise to peaks between 195 nm and 166 nm [18]. Measurements of vapour from 5 μ l of acetone in a 1 mm cell produced resolvable peaks in the HT signal at $\sim$ 190.7 nm, $\sim$ 195 nm when measured on a conventional machine and one SRCD instrument (data not shown). However, on conventional instruments the slits need to be fully open at lower wavelengths to increase the light flux to enable the measurement and this creates uncertainty in the wavelengths measured. For SRCD instruments, calibration at much lower wavelengths can be achieved by observing a series of electric dipole forbidden nitrogen transitions between 145 nm and 127 nm [19]. In this study, six distinct peaks were observed in the HT signal at 145, 142, 136, 133, 130 and 127 nm using two SRCD instruments (data not shown).

In summary, in this paper a number of parameters important for producing accurate and reproducible CD spectra were examined. Methods for improving the accuracy and comparability of CD spectral magnitudes and peak positions were presented. Hence, this paper provides practical guidance for “good practice” in the measurement of CD data.

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