Review Article

In Vivo Tracking of Cell Therapies for Cardiac Diseases with Nuclear Medicine

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Eventhoughheartdiseasesareamongstthemaingcausesofmortalityandmorbidityintheworld,existingtreatmentsarelimitedin
restoringcardiaclesions.Celltransplantations,originallydevelopedforthetreatmentofhematologicailments,arepresentlybeing
exploredinpreclinicalandclinicaltrialsforcardiacdiseases.Nonetheless,littleisknownaboutthepossibleefficacyandmechanisms
forthesetherapiesandtheyaret hecenterofcontinuousinvestigation.Inthisscenario,noninvasiveimagingtechniqueslead
togreatercomprehensionofcelltherapies.Radiopharmaceuticalcelllabeling,firstlydevelopedtotrackleukocytes,hase been
successfullytoevaluatethemigrationofcelltherapiesformyocardialdiseases.Asubstantialriseintheamountofreportsemploying
thismethodologyhas taken place in the previous years. We will review the diverse radiopharmaceuticals, imaging modalities, and
results of experimental and clinical studies published until now. Also, we report on current limitations and potential advances of
radiopharmaceutical labeling for cell therapies in cardiac diseases.

1. Introduction

Cardiovascular ailments are still the greatest causes of mor-
bidity and mortality in the world, with significant financial
and social consequences [1, 2]. Despite recent medical and
surgical advances in the past decades, currently there are
no effective therapies to allow cardiac regeneration [3].
On this scenario, experimental studies have indicated that
cell therapies may target cardiac regeneration in acute and
chronic myocardial diseases [3]. Although clinical studies
have already been carried out, the efficacy and potential
mechanisms of cell therapies for cardiac diseases are still
under continuous investigation [4–6]. Possible mechanisms
of action of cell therapies include the secretion of paracrine
factors that reduce cardiomyocyte death, improve local
microcirculation, and decrease the amount of fibrous tissue,
which may improve heart function [3].

Noninvasive imaging modalities have the potential of
providing better understanding of the biological process and
the effectiveness of cell therapies for cardiac diseases [7].

One of the main applications of these techniques is to track
the migration of cell therapies [7]. Among the different
imaging techniques available, Nuclear Medicine has become
one of the most employed techniques, due to its favorable
characteristics, such as the availability of different radiophar-
maceuticals and its high sensitivity [8]. In this paper, we
will review preclinical and clinical studies that used Nuclear
Medicine to evaluate cell migration and discuss important
issues in this area.

2. Use of Radiopharmaceuticals

for Cell Labeling

In the past decades, labeled leukocyte scintigraphy has
become an important method to locate sites of infection
and inflammation in the body [9, 10]. The development of
this method had been a key landmark in the history of
Nuclear Medicine. Conventional techniques include two-
dimensional planar scintigraphy and three-dimensional
single photon emission computed tomography (SPECT). Additionally, SPECT images may be acquired together with a computed tomography, resulting in hybrid SPECT/CT images [11]. This technique allows a better location of the findings of Nuclear Medicine, thus increasing the sensitivity and specificity of the method [11].

A variety of labeling methods with radionuclides has been created and used to study cell distribution in the body [12]. Currently, technetium-99m (99mTc) is the most commonly utilized radionuclide in the world, due to favorable properties such as its decay by gamma emission with an energy of 140 keV and a 6-hour half-life, optimum physical characteristics for SPECT, allowing images for up to 24 hours after injection [9]. Radionuclide indium-111 (111In) may also be used for cell labeling in SPECT, for example, through compounds 111In-oxine and 111In-tropolone [9].

The radionuclide fluorine-18 (18F) has a half-life of approximately 110 minutes and is the most frequently utilized in positron emission tomography (PET) and hybrid PET/CT, mainly in the radiopharmaceutical 18F-fluorodeoxyglucose (18F-FDG) [12]. PET has better spatial resolution than SPECT and allows the quantification of the standardized uptake value (SUV) [12, 13]. Zirconium-89 (89Zr) is another promising radionuclide for cell labeling in PET that has a 78.4-hour half-life and may allow cell tracking for two to three weeks [14].

Tracking cells with SPECT and PET may be separated in two strategies: direct and indirect [15]. Direct tracking is achieved by labeling cells with a radiotracer in vitro with subsequent cell administration [7, 15]. The most widely used radionuclides for direct labeling are 99mTc and 111In to perform SPECT and 18F to perform PET [9, 16]. Indirect cell tracking may be achieved employing reporter gene/probe systems that have been the topic of exceptional reviews [8, 17]. For instance, a lentivirus may be used to deliver a reporter gene for expression of herpes simplex virus truncated thymidine kinase (TK) that catalyzes a reaction leading to the accumulation of the probe 18F-9-[4-fluoro-3-(hydroxymethyl)butyl]guanine derivatives (18F-FHBG) for PET imaging [17]. Another example of reporter gene is the Sodium Iodide Sympporter (NIS), a cell surface protein expressed usually in thyroid cells, salivary glands, mammary glands, and choroid plexus, but not in organs such as the heart [18]. Cells overexpressing NIS will capture 99mTc and iodine-123 (123I) for SPECT, as well as iodine-124 (124I) for PET, allowing the evaluation of viable cell homing in the heart after transplantation [18].

3. Preclinical Studies

3.1. Direct Cell Labeling. We identified 31 published articles that used direct cell labeling to track the migration and homing of cell therapies in preclinical models of heart diseases, all of them for myocardial infarction (Table I).

3.1.1. Effect on Cell Viability, Metabolic Activity, and Migration. Although the use of 111In in radiopharmaceuticals allows cell tracking for longer periods in comparison to 99mTc, it has high energy (171 and 245 keV), which leads to images of lower resolution and greater cell dose that may decrease cell viability [19–21]. 111In can affect the viability, metabolic activity, and migration of stem cells due to internalization of Auger electrons emitted at close distances. These electrons may lead to considerable toxicity to target cells reducing cell viability [10, 19–21].

Jin et al. carried out an interesting study where they evaluated the viability of bone marrow-derived mesenchymal stem cells (BM-MSCs) labeled with 111In [22]. Distinct samples with 5 × 10^6 cells were labeled 0.1 to 18 MBq of 111In-tropolone. The authors reported that cells had 100% viability when incubated with up to 0.9 MBq, which corresponded to 0.14 Bq per cell.

Brenner et al. [19] reported the impact of labeling human CD34+ hematopoietic progenitor cells (HPCs) with 111In-oxine. HPCs (1 × 10^6/mL) were incubated with 30 MBq of 111In-oxine for 1 hour to assess cell viability at 1, 24, 48, and 96 hours. Although no significant changes were observed at 24 hours after labeling, after 48 and 96 hours the number of dead cells increased. Furthermore, cell migration was quickly reduced after 24 hours.

Suhett et al. [23] studied the binding sites for 99mTc in rat bone marrow mononuclear cells (BM-MNCs). BM-MNCs were labeled with 45 MBq of 99mTc-O4-. After being labeled, cells were carefully disrupted and differentially centrifuged for organelle separation. Viability of the labeled cells was 93% and most of the radiation remained in the supernatant comprised of the cytosol and membrane bound ribosomes.

18F-FDG is regarded as the gold standard for the assessment of myocardial viability. 18F-FDG is a glucose analogue that enters cardiomyocytes through glucose transporters (GLUTs) such as GLUT1 and GLUT4. Within the cell, 18F-FDG suffers phosphorylation by hexokinase and converts to 18F-glucose 6-phosphate. Because it is not metabolized, it is retained within the cell. Preclinical studies made by Chan and Abraham reported that 18F-FDG caused no interference with proliferation of cardiac-derived stem/progenitor cells (CPCs) [7]. Similarly, Wolfs et al. found no significant changes to the ultrastructure and differentiation of mouse MSCs and rat multipotent adult progenitor cells [24].

Hexadecyl-4-[18F] fluorobenzoate (18F-FHB) is a lipophilic radiopharmaceutical that is absorbed through the cell membrane, allowing cell tracking by PET. Zhang et al. [25] compared the labeling of human peripheral blood-derived circulating progenitor cells (CPCs) with 18F-HFB and 18F-FDG in mice after myocardial infarction. Cells were injected close to the site of cardiac injury. The images were made in Micro-PET 10 min and 2 and 4 hours after injection. 13N-NH3 was used to outline the liver and the heart. Labeling with 18F-HFB showed no reduction in cell viability with 14.8–22.2 MBq of radioactivity in 2 × 10^6; however, higher activities (185–259 MBq) resulted in significant cell death. After 24 hours, the reduction of viability in 18F-HFB-CPCs was 13.3%, whereas in controls it was 6.9%. After 5 days cell viability decreased for both groups: 18F-HFB-CPCs (10.4%) and 18F-FDG-CPCs (14.7%).
Table 1: Preclinical studies that used direct radiopharmaceutical labeling for cell therapies in models of myocardial infarction.

<table>
<thead>
<tr>
<th>Study reference</th>
<th>Radiopharmaceutical used for cell tracking</th>
<th>Time window of cell injection after lesion induction</th>
<th>Animals</th>
<th>Cell type</th>
<th>Route(s)</th>
<th>Number of cells injected</th>
<th>Radionuclide activity</th>
<th>Time points of analysis after cell therapy</th>
</tr>
</thead>
<tbody>
<tr>
<td>Aicher et al., 2003 [33]</td>
<td>$^{111}$In-oxine</td>
<td>24 h</td>
<td>Athymic nude rats</td>
<td>Human EPCs</td>
<td>Intravenous Intraventricular</td>
<td>$1 \times 10^6$</td>
<td>15 Bq/cell</td>
<td>1, 24, 48, and 96 hours</td>
</tr>
<tr>
<td>Barbash et al., 2003 [34]</td>
<td>$^{99m}$Tc-HMPAO</td>
<td>2 days or 10–14 days</td>
<td>Athymic nude rats</td>
<td>Rat BM-MSC</td>
<td>Intravenous Intraventricular</td>
<td>$4 \times 10^6$</td>
<td>Not specified</td>
<td>Not specified</td>
</tr>
<tr>
<td>Brenner et al., 2004 [19]</td>
<td>$^{111}$In-oxine</td>
<td>24 hours</td>
<td>Athymic nude rats</td>
<td>Human HPCs</td>
<td>Intraventricular</td>
<td>Not specified</td>
<td>30 Bq/cell</td>
<td>1, 24, 48, and 96 hours</td>
</tr>
<tr>
<td>Zhou et al., 2005 [35]</td>
<td>$^{111}$In-oxine</td>
<td>Immediately</td>
<td>Sprague-Dawley rats</td>
<td>Rat H9c2</td>
<td>Intramyocardial</td>
<td>$3-4 \times 10^6$</td>
<td>3.7 Bq/cell</td>
<td>2, 24, 48, 72, and 96 hours</td>
</tr>
<tr>
<td>Kraitchman et al., 2005 [30]</td>
<td>$^{111}$In-oxine</td>
<td>72 hours</td>
<td>Dogs</td>
<td>Canine BM-MSCs</td>
<td>Intravenous</td>
<td>$1.6 \times 10^8$</td>
<td>0.4 Bq/cell</td>
<td>Same day to 8 days</td>
</tr>
<tr>
<td>Hou et al., 2005 [97]</td>
<td>$^{111}$In-oxine</td>
<td>6 days</td>
<td>Pigs</td>
<td>Human BM-MNCs</td>
<td>Intracoronary Intramyocardial IRV</td>
<td>$1 \times 10^7$</td>
<td>1,85 Bq/cell</td>
<td>1 hour</td>
</tr>
<tr>
<td>Tran et al., 2006 [37]</td>
<td>$^{111}$In-oxine</td>
<td>3 months</td>
<td>Wistar rats</td>
<td>Rat BM-MSCs</td>
<td>Intramyocardial</td>
<td>$2 \times 10^6$</td>
<td>7.5 Bq/cell</td>
<td>2 days</td>
</tr>
<tr>
<td>Tran et al. 2006 [38]</td>
<td>$^{111}$In-oxine</td>
<td>1 month</td>
<td>Wistar rats</td>
<td>Rat BM-MSCs</td>
<td>Intramyocardial</td>
<td>$2 \times 10^6$</td>
<td>7.5 Bq/cell</td>
<td>7 days</td>
</tr>
<tr>
<td>Shen et al., 2007 [36]</td>
<td>$^{111}$In-oxine</td>
<td>Immediately</td>
<td>Sprague-Dawley rats</td>
<td>Rat embryonic cardiomyoblasts</td>
<td>Intramyocardial</td>
<td>$3-4 \times 10^6$</td>
<td>3.7 Bq/cell</td>
<td>30 minutes</td>
</tr>
<tr>
<td>Tran et al., 2007 [39]</td>
<td>$^{111}$In-oxine</td>
<td>4 months</td>
<td>Wistar rats</td>
<td>Rat BM-MSCs</td>
<td>Intramyocardial</td>
<td>$2 \times 10^6$</td>
<td>7.5 Bq/cell</td>
<td>48 h</td>
</tr>
<tr>
<td>Qian et al., 2007 [50]</td>
<td>$^{18}$F-FDG</td>
<td>7 days</td>
<td>Chinese mini-pigs</td>
<td>Porcine BM-MNCs</td>
<td>Intracoronary</td>
<td>$1.0 \times 10^9$</td>
<td>0.185 Bq/cell</td>
<td>1 hour</td>
</tr>
<tr>
<td>Doyle et al., 2007 [51]</td>
<td>$^{18}$F-FDG</td>
<td>48 hours</td>
<td>Pigs</td>
<td>Porcine CPCs</td>
<td>Intracoronary</td>
<td>$3 \times 10^7$</td>
<td>Not specified</td>
<td>1 hour</td>
</tr>
<tr>
<td>Lutz et al., 2008 [31]</td>
<td>$^{111}$In-tropolone</td>
<td>24 h</td>
<td>C57BL/6 mice</td>
<td>Intravenous</td>
<td>Intracoronary</td>
<td>$1 \times 10^6$</td>
<td>0.037 Bq/cell</td>
<td>24 and 72 hours</td>
</tr>
<tr>
<td>Tossios et al., 2008 [53]</td>
<td>$^{111}$In-tropolone</td>
<td>5 days</td>
<td>Pigs</td>
<td>Porcine BM-MNCs</td>
<td>Intracoronary Intramyocardial</td>
<td>$1 \times 10^8$</td>
<td>Not specified</td>
<td>Immediately; 1–24 hours</td>
</tr>
<tr>
<td>Blackwood et al. 2009 [26]</td>
<td>$^{111}$In-tropolone</td>
<td>Immediately</td>
<td>Dogs</td>
<td>Canine BM-MSCs</td>
<td>Intramyocardial</td>
<td>$3.08 \times 10^7$</td>
<td>1.7 Bq/cell</td>
<td>Same day and 2 weeks</td>
</tr>
<tr>
<td>Terrovitis et al. 2009 [41]</td>
<td>$^{18}$F-FDG</td>
<td>Immediately</td>
<td>Wistar Kyoto rats</td>
<td>Rat CDCs</td>
<td>Intramyocardial</td>
<td>$2 \times 10^6$</td>
<td>Not specified</td>
<td>Not specified</td>
</tr>
<tr>
<td>Mäkelä et al., 2009 [54]</td>
<td>$^{111}$In-oxine</td>
<td>30 minutes</td>
<td>Pigs</td>
<td>Porcine BM-MNCs</td>
<td>Intramyocardial</td>
<td>$2 \times 10^6$</td>
<td>0.185 Bq/cell</td>
<td>Not specified; 2 and 24 hours and 6 days</td>
</tr>
</tbody>
</table>
Table 1: Continued.

<table>
<thead>
<tr>
<th>Study reference</th>
<th>Radiopharmaceutical used for cell tracking</th>
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<th>Cell type</th>
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<th>Radionuclide activity</th>
<th>Time points of analysis after cell therapy</th>
</tr>
</thead>
<tbody>
<tr>
<td>Mitchell et al., 2010 [44]</td>
<td>$^{111}$In-tropolone</td>
<td>Same day and 7 days</td>
<td>Dogs</td>
<td>Canine EPC</td>
<td>Epicardial and Endocardial</td>
<td>$2.8 \times 10^7$</td>
<td>0.1 Bq/cell</td>
<td>30–40 minutes 4 and 10 and up to 15 days</td>
</tr>
<tr>
<td>Forest et al., 2010 [55]</td>
<td>$^{99m}$Tc</td>
<td>5 days</td>
<td>Pigs</td>
<td>BM-MNCs</td>
<td>Intravenous and Intracoronary</td>
<td>$1 \times 10^7$ (intracoronary)</td>
<td>Not specified</td>
<td>1 and 24 hours</td>
</tr>
<tr>
<td>Danoviz et al., 2010 [27]</td>
<td>$^{99m}$Tc-HMPAO</td>
<td>24 hours</td>
<td>Lewis rats</td>
<td>Rat ADSCs</td>
<td>Intramyocardial</td>
<td>$1 \times 10^6$ (intravenous)</td>
<td>Not specified</td>
<td>Not specified Immediately; 4 and 10 days 10 min, 2 and 4 hours</td>
</tr>
<tr>
<td>Sabondjian et al., 2012 [46]</td>
<td>$^{111}$In-tropolone</td>
<td>Not specified</td>
<td>Dogs</td>
<td>Canine EPCs</td>
<td>Intramyocardial</td>
<td>Not specified</td>
<td>Not specified</td>
<td>Not specified Immediately; 4 and 10 days 10 min, 2 and 4 hours</td>
</tr>
<tr>
<td>Zhang et al., 2012 [25]</td>
<td>$^{18}$F-HFB</td>
<td>14 days</td>
<td>Sprague-Dawley rats</td>
<td>Human CPCs</td>
<td>Epicardial and Endocardial</td>
<td>$2 \times 10^6$</td>
<td>7.4 to 11.1 Bq/cell</td>
<td>4 hours</td>
</tr>
<tr>
<td>Mitchell et al., 2013 [45]</td>
<td>$^{111}$In-tropolone</td>
<td>First: 4 hours or 7 days/second: 4 weeks later</td>
<td>Dogs</td>
<td>Canine EPCs</td>
<td>Intramyocardial</td>
<td>$3 \times 10^7$</td>
<td>0.1 Bq/cell</td>
<td>Same day and 4, 10, and 15 days</td>
</tr>
<tr>
<td>Maureira et al., 2013 [47]</td>
<td>$^{111}$In-oxine</td>
<td>4 months</td>
<td>Wistar rats</td>
<td>Rat BM-MSCs</td>
<td>Intramyocardial</td>
<td>$2 \times 10^6$</td>
<td>75 Bq/cell</td>
<td>48 hours</td>
</tr>
<tr>
<td>Lang et al., 2013 [42]</td>
<td>$^{18}$F-FDG</td>
<td>5 minutes</td>
<td>C57BL6/N wild-type mice</td>
<td>Murine ESCs</td>
<td>Intramyocardial</td>
<td>$3 \times 10^6$</td>
<td>0.8 Bq/cell</td>
<td>25 minutes and 2 hours</td>
</tr>
<tr>
<td>Elhami et al., 2013 [49]</td>
<td>$^{18}$F-FDG</td>
<td>Immediately or 7 days</td>
<td>Lewis rats</td>
<td>Rat ADSCs</td>
<td>Intramyocardial and Intra-ventricular, intravenous</td>
<td>$4.5$–$6.0 \times 10^6$</td>
<td>20 Bq/cell</td>
<td>4 hours</td>
</tr>
<tr>
<td>Garikipati et al., 2014 [32]</td>
<td>$^{99m}$Tc-HMPAO</td>
<td>7 days</td>
<td>Sprague-Dawley rats</td>
<td>Rat FC-MSCs</td>
<td>Intramyocardial</td>
<td>$2 \times 10^6$</td>
<td>37 Bq/cell</td>
<td>6 hours</td>
</tr>
<tr>
<td>Lang et al., 2014 [43]</td>
<td>$^{18}$F-FDG</td>
<td>5 minutes</td>
<td>C57BL6/N wild-type mice</td>
<td>Murine ESCS and fibroblasts</td>
<td>Intramyocardial</td>
<td>$3 \times 10^6$</td>
<td>0.8 Bq/cell</td>
<td>2 hours</td>
</tr>
<tr>
<td>Kim et al., 2015 [48]</td>
<td>$^{124}$I-HIB</td>
<td>Not specified</td>
<td>Sprague-Dawley rats</td>
<td>Rat ADSCs</td>
<td>Intramyocardial</td>
<td>$5 \times 10^6$</td>
<td>0.2 to 0.3 Bq/cell</td>
<td>1 day ($^{18}$F-FDG) and 9 days ($^{124}$I-HFB)</td>
</tr>
<tr>
<td>Keith et al., 2015 [52]</td>
<td>$^{111}$In-oxine</td>
<td>1-2 months</td>
<td>Pigs</td>
<td>Human CDGs</td>
<td>Intramyocardial</td>
<td>$1 \times 10^7$</td>
<td>277 Bq/cell</td>
<td>24 hours</td>
</tr>
<tr>
<td>Bansal et al., 2015 [14]</td>
<td>$^{88}$Zr</td>
<td>1 hour</td>
<td>Mice</td>
<td>Human MSCs</td>
<td>Intramyocardial</td>
<td>$2 \times 10^6$</td>
<td>0.37 Bq/cell</td>
<td>2, 5, and 7 days</td>
</tr>
</tbody>
</table>

$^{111}$In: indium-111; $^{18}$F: fluorine-18; $^{88}$Zr: zirconium-88; $^{99m}$Tc: technetium-99m; ADSCs: adipose tissue-derived stem cells; BM-MNCs: bone marrow mononuclear cells; BM-MSCs: bone marrow mesenchymal stem cells; CDCs: cardiac-derived stem/progenitor cells; CPCs: circulating progenitor cells; EPCs: endothelial progenitor cells; ESCs: embryonic stem cells; FC-MSCs: mesenchymal stem cells derived from rat fetal heart; FDG: fluorodeoxyglucose; HFB: hexadecyl-4-fluorobenzoate; HIB: hexadecyl-4-tributylstannylbenzoate; HMPAO: hexamethylpropyleneamine oxime; IRV: interstitial retrograde coronary venous; PB-MNCs: peripheral blood mononuclear cells.
3.1.2. Radionuclide Leakage and Labeling Efficiency. Quantifying in vivo cell transplant survival may be difficult, and radionuclide leakage is an important issue that should be taken into account [26]. Radionuclide leakage may occur from viable cells and cellular debris [26]. Many authors applied different in vivo experiments to determine cell death, radiolabel leakage, and cell survival [26, 27]. Another issue to be evaluated is the normal turnover of the cells, where one may label cells and administer them in order to study the clearance characteristics from viable cells that did not die in vivo [26].

Blackwood et al. [26] quantified the survival of BM–MSCs labeled with $^{111}$In. In transplanted into the canine myocardium. The authors also evaluated the clearance of lysed $^{111}$In labeled cells. Serial SPECT images were acquired after direct epicardial injection to determine the time-dependent radiolabel clearance. The average long biologic half-life for labeled cells was 74.3 hours and for lysed cells was 19.4 hours.

The labeling efficiency of direct labels differs between different methods and needs to be taken into account [28]. For instance, it has been reported that the labeling with $^{99m}$Tc-tropolone was more effective and stable in comparison to $^{99m}$Tc-hexamethylpropyleneamine oxime ($^{99m}$Tc-HMPAO) [29]. In another example, Zhang et al. reported that $^{18}$F-HFB labeling showed a higher efficiency when compared with $^{18}$F-FDG [25].

3.1.3. Biodistribution after Intravenous Injection. Kraitchman et al. [30] investigated the migration of BM–MSCs labeled with $^{111}$In-oxine, by intravenous route, 72 hours after the induction of lesion myocardial infarction in dogs. SPECT imaging was carried out up to 8 days after cell transplantation. Uptake on the same day of cell therapy was mainly restricted to the lungs in infarcted animals and control animals with low uptake in the heart. At 24 hours, uptake remained constant in the heart, decreased in the lungs, and increased in the liver and spleen.

Lutz et al. [31] studied the migration of systemically injected bone marrow-derived cells in mice after myocardial infarction. After induction of the infarction, animals received intramyocardial injections of stem cell factor (SCF) in peri-infarcted areas. Cells were labeled with $^{111}$In-oxine and injected in the tail vein 24 hours after the infarction. Animals were sacrificed and hearts removed for analysis in a gamma counter 24 or 72 hours later. The analysis indicated that intramyocardial injections of SCF significantly increased myocardial uptake in comparison with infarcted animals that received saline injections and with sham-operated animals at both time points.

Garikipati et al. [32] investigated the efficacy of therapy with fetal cardiac mesenchymal stem cells (FC–MSCs) in rats after myocardial infarction. FC–MSCs were isolated and cultured from fetal rat hearts. Seven days after the induction of the lesion, mice were divided into FC–MSC or saline group. Cells were labeled with $^{99m}$Tc-HMPAO and injected into the tail vein. Multipinhole gated SPECT/CT was carried out six hours after the intravenous infusion and $^{99m}$Tc labeled cells were mainly present in the lungs, with focal homing in the heart.

3.1.4. Biodistribution after Intraventricular Injection. Brenner et al. [19] performed intraventricular injections of human HPCs into the left ventricular cavity of rats after myocardial infarction. SPECT was performed 1, 24, 48, and 96 hours after transplantation. Liver, kidneys, and spleen combined had 37% and lungs 17% of whole body uptake 1h after cell transplantation. Twenty-four hours after the injection, lung uptake was no longer detected, while homing to the liver, kidneys, and spleen increased to 57%. Only 1% of the injected activity was found in the heart of transplanted animals.

Aicher et al. investigated the transplantation of $^{111}$In-oxine labeled endothelial progenitor cells (EPCs) into rats after myocardial infarction [33]. Labeled cells were delivered in the tail vein or in the left ventricular cavity. Pinhole SPECT was performed after cell administration. Total uptake in the liver, kidneys, and spleen was 71% after 96 hours, while myocardial uptake was only 1-2% after intravenous injection and 3-5% after intravitreal myocardial infusion.

Barbash et al. evaluated the effectiveness and feasibility of systemic administration of BM–MSCs in rats following myocardial infarction. Cells were labeled by incubation with $^{99m}$Tc-HMPAO [34]. Three injection methods were studied. The first approach was by infusion of BM–MSCs in the femoral vein. In the second strategy, BM–MSCs were infused directly into the left ventricle. In the third group, cells were injected into the right ventricle, but all animals died from pulmonary embolism. Images were acquired 4 hours after the infusion and indicated that rats with myocardial infarction had higher uptake of $^{99m}$Tc labeled cells in the heart than sham animals. Moreover, intravenous infusion resulted in lower myocardial homing due to pulmonary cell retention.

3.1.5. Biodistribution after Intramyocardial Injection. Zhou et al. [35] investigated the distribution of rat embryonic cardiomyoblasts (H9c2) cells after labeling with $^{111}$In-oxine rats after myocardial infaract. Cells were intramyocardially transplanted around the infarcted region immediately after induction of the lesion and SPECT images acquired 2, 24, 48, 72, and 96 hours. The authors reported that cell uptake was detected in the injection site up to 96 hours after administration.

Shen et al. [36] used magnetic resonance imaging (MRI) and SPECT imaging to monitor H9c2 cell transplantation in rats after myocardial infarction. Myocardial infarction was induced and $^{111}$In labeled cells were injected in regions close to the injured site. MRI was performed 5–7 days after SPECT images. Through a coregistration algorithm, it was possible to carry out the fusion of SPECT-MRI images. The authors were able to monitor the uptake of $^{111}$In-oxine labeled cells and the perfusion in $^{99m}$Tc-sestamibi images.

Tran et al. [37–39] evaluated in a series of studies the migration of $^{111}$In-oxine labeled BM–MSCs in rats one to four months after myocardial infarction in rats. Cells were injected in the infarcted areas. Cell distribution was compared with $^{99m}$Tc-sestamibi imaging of myocardial perfusion using
a 17-segment division of the left ventricle. The authors concluded that BM-MSCs homing was heterogeneous and did not match in all occasions the infarcted regions [37–39].

Wisenberg et al. [40] evaluated dogs using both imaging of 111In-tropolone labeled cells and late gadolinium enhancement cardiac MRI for up to 12 weeks after a 3-hour coronary occlusion. The animals were injected with BM-MSCs and imaged at day 0 (surgery) and after 4, 7, 10, and 14 days. SPECT imaging indicated an effective biological clearance half-life from the injection site of ~5 days, while cardiac MRI demonstrated a pattern of progressive infarct clearance half-life from the injection site of 1–5 days, while cardiac MRI demonstrated a pattern of progressive infarct half-life from the injection site of 1–5 days.

Terrovitis et al. [41] labeled rat CDCs with 18F-FDG to monitor cell therapy in rats after myocardial infarction. CDCs were injected intramyocardially. In other groups of animals, the effects of fibrin glue, bradycardia (by adenosine injection), and induction of cardiac arrest on cell homing were investigated. One hour after cell transplantation without additional measures, PET indicated that mean myocardial homing was 17.8%. Adenosine injection was able to decrease the heart rate and double cell mean cell homing to 35.4%. A comparable enhancement in cell homing was seen when the authors applied fibrin glue epicardially and mean cell homing increased to 37.5%. However, the greatest increase was seen after induction of cardiac arrest, when mean homing increased to 75.6%.

Lang et al. [42, 43] studied the distribution of 18F-FDG labeled murine embryonic stem cells (ESCs) or fibroblasts in C57BL/6/N mice after myocardial infarction, five minutes after the infarct ESCs or fibroblasts were injected intramyocardially [42, 43]. Images were made in a preclinical PET. The authors reported that the percentages of uptake in the heart were 5.2–5.3% after 25 minutes, 4.8–5.0% after 1 hour, and 5.6–5.7% after 2 hours.

Danoviz et al. assessed the transplantation of adipose tissue-derived stem cells (ADSCs) with two biopolymers, fibrin and collagen, in murine model of acute myocardial infarction [27]. Cells were labeled with 99mTc-HMPAO. Twenty-four hours after induction of the lesion, the animals were injected with cells suspended in 100 mL of carrier by intracoronary route. Cells were infused in the border of the lesion with fibrin, collagen, or culture medium. Radioactivity counting of the organs revealed high levels of radioactivity in the liver, kidneys, and lungs. Both biopolymers increased cellular retention, but the collagen group showed higher uptake (26.8%) when compared to fibrin and culture medium (13.7% and 4.84%, resp.).

Mitchell et al. [44, 45] and Sabondjian et al. [46] assessed the migration of EPCs in canine models of myocardial infarction up to 7 days after induction of the lesion. EPCs were labeled with 111In-tropolone and injected by epicardial and endocardial routes. SPECT imaging was performed up to 15 days after cell transplantation. The authors reported that cell homing occurred in hyperperfused areas and that epicardial and endocardial injections led to similar uptake.

Maureira et al. [47] developed an in vivo technique with pinhole SPECT to monitor stem cell migration after myocardial infarction in rats. After coronary occlusion, autologous BM-MSCs were labeled with 111In-oxine. An intramyocardial injection was administered in the infarcted region. Two days after the procedure, 99mTc-sestamibi was injected to compare homing of 111In labeled cells and myocardial perfusion. Left ventricle perfusion and function in all animals were monitored 2 days before cell therapy and 1–6 months after therapy using a pinhole gated SPECT. Significant improvements in cardiac perfusion were observed in injured areas and also in areas not transplanted.

Kim et al. [48] studied the homing of ADSCs after direct labeling with 124I-hexadecyl-4-tributylstannylenzooate (124I-HIB) or 18F-FDG in rats after myocardial infarction. Cells were labeled with 124I-HIB or 18F-FDG. An intramyocardial injection was performed in the infarct site. 124I-HIB labeled cells were seen at the infarct area and monitored for up to 3 days in lesioned animals. The authors reported that labeling efficiency with 124I-HIB was higher than with 18F-FDG, indicating it could be a good method to monitor stem cell homing.

Elhami et al. [49] investigated the migration of 18F-FDG labeled ADSCs after myocardial infarction in rats. Labeling was carried out with 18F-FDG. Immediately after the infarct induction, cell transplantation was carried out by intramyocardial, intraventricular, or intravenous route. In another group, cells were injected intramyocardially 7 days after the infarct. The authors reported that the intravenous route led to lower cell homing in the heart (1.2% of infused ADSCs) 4 hours after cell transplantation. Intraventricular injection led to an uptake of 3.5% in the heart, while intramyocardial injection led to the highest myocardial cell homing (14%). Interestingly, in the group that received an intramyocardial cell injection 7 days after the myocardial infarction, cell homing was lower (4.5%) than the group that received cells immediately after the infarct induction.

3.1.6. Biodistribution after Intracoronary Injection. Qian et al. [50] determined the distribution of BM-MNCs after myocardial infarction in Chinese mini-pigs. Cells were labeled with 18F-FDG and injected intramyocardially 7 days after the infarct. One hour after cell transplantation, 6.8% of the whole body uptake was located in the infarct site. Liver and spleen showed more than 90% of the uptake.

Doyle et al. [51] tracked CPCs in pigs after acute myocardial infarction. CPCs were labeled with 18F-FDG. One group received CPCs divided into 3 cycles after a balloon catheter was positioned and inflated in the lesioned artery. A second group received a single bolus infusion of CPCs without balloon inflation. The authors reported that one hour after cell transplantation the group that received the infusion in 3 cycles with balloon occlusion had lower uptake in the heart than the group that received a single bolus injection (8.7% versus 17.8%, resp.). The majority of activity (>60%) was concentrated in the lungs after 1 hour in both groups, and there was moderate uptake in the liver and spleen.

Keith et al. [52] investigated the impact of using intracoronary human CDC injection on cell homing in a pig model of myocardial infarction. Cells were injected with...
or without balloon inflation after labeling with $^{111}$In-oxine. SPECT was carried out 24 hours after cell transplantation. The authors reported that the injection with balloon occlusion led to similar myocardial homing as the one without balloon occlusion (5.41% versus 4.87%, resp.) and concluded that the risk involved in the coronary occlusion approach would not be warranted.

Hou et al. evaluated the distribution of peripheral blood mononuclear cells (PB-MNCs), labeled with $^{111}$In, in pigs after myocardial infarction. The lungs had 1%, 3%, and 3% of the uptake, while myocardial uptake was 2.6%, 3.2%, and 11% after intracoronary, interstitial retrograde coronary venous, or intramyocardial injections, respectively.

Tossios et al. [53] monitored the distribution of BM-MNCs following induction of myocardial infarction in pigs. After labeling with $^{111}$In-tropolone, cells were injected by intramyocardial or by intracoronary route with or without balloon occlusion. One hour after injection, 20.7%, 4.1%, and 6.1% of the uptake were located in the heart after intramyocardial, intracoronary without balloon, and intracoronary with balloon infusions, respectively. Twenty-four hours later, myocardial uptake was 15.0%, 3.0%, and 3.3%, respectively. The lungs, liver, and spleen had 50%, 10%, and 5% of the uptake in the whole body, respectively.

Mäkelä et al. [54] evaluated the migration of BM-MNCs in a pig model of myocardial infarction. Cells were labeled with $^{111}$In-oxine and transplanted by intramyocardial or intracoronary routes 30 minutes after induction of the lesion. SPECT was acquired 2 and 24 hours after transplantation and biopsies from different organs were also performed to allow gamma counting. The authors reported that the intracoronary injection led to <15% of the cardiac uptake observed after intramyocardial injection, while lung uptake after intramyocardial injection was <15% of the pulmonary uptake observed after intracoronary infusion.

Forest et al. studied a preclinical model of myocardial infarction in pigs [55]. Seven days after induction of the lesion, BM-MNCs were labeled with $^{99m}$Tc. Animals were divided into three groups: control group, intracoronary injection, and intravenous injection of $^{99m}$Tc labeled cells. Intravenous administration led to higher cell accumulation in the lungs, while intracoronary injection led to greater myocardial uptake.

3.2. Indirect Radiolabeling: Reporter Gene/Probe Systems

Reporter gene/probe imaging for SPECT and PET has been applied to evaluate the survival of transplanted cells in animal models of cardiac diseases [8]. Some of the disadvantages of using reporter genes include the possible immunogenicity of the viral reporter gene, which limits the application of the technique in humans [7]. Moreover, the stability of transfection and expression must be improved and the potential interference with stem cell function and differentiation from vector transfection or transduction must be minimized [56]. We identified 9 published articles that used indirect cell tracking to evaluate the migration and homing of cell therapies in preclinical models of heart diseases, all of them for myocardial infarction (Table 2).
3.2.1. Biodistribution after Intramyocardial Injection. Gyöngyösi et al. [57] used reporter gene imaging to monitor the migration of BM-MSCs in a pig model of myocardial infarction. Cells transfection was performed with a lentivirus for expression of TK. Sixteen days after the infarction, a group of animals received BM-MSCs by intramyocardial injection. Then, $^{18}$F-FHBG was injected 30 hours and 7 days after cell transplantation for *in vivo* imaging. The authors reported that there was a decrease in myocardial uptake of $^{18}$F-FHBG after 7 days in comparison with the 30-hour images, as well as mild increase in pericardial and pleural uptake.

Terrovitis et al. [58] transfected rat CDCs with a lentivirus to express the NIS gene. *In vivo* images were obtained after intramyocardial cell injection in mice after myocardial infarction. An injection of $^{99m}$Tc for SPECT imaging or $^{124}$I for PET imaging was used to evaluate the expression of NIS gene in transplanted CDCs. The authors were able to detect the transplanted CDCs with a threshold of approximately $10^4$ cells. Cell homing was seen up to 6 days after CDC transplantation but less than 5% of cells remained in the heart, due to migration to the lungs and systemic circulation.

Lee et al. [59] investigated the homing of canine iPSCs after cell transplantation in dogs. Cells were injected intramyocardially 30 minutes after the induction of myocardial infarction. The authors injected an activity of approximately 536 MBq of $^{18}$F-FHBG and carried out PET/CT 8 hours after cell transplantation. Imaging revealed cell homing to the anterior myocardial wall.

Liu et al. [60] and Lan et al. [61] analyzed the migration of human CDCs in rats after myocardial infarction in severe combined immunodeficiency (SCID) Beige mice. A total of $1 \times 10^6$ cells transfected with a TK reporter gene were injected by intramyocardial route immediately after the induction of myocardial infarction. On days 1, 7, 14, 21, and 28 after cell therapy, an activity of 7.4 MBq of $^{18}$F-FHBG was injected to allow PET imaging. A gradual decrease in the amount of surviving cells was noticed during the follow-up. Interestingly, the authors reported that early cell homing predicted ensuing functional improvement [60].

Using reporter genes, Templin et al. [62] were able to monitor human induced pluripotent stem cells (iPSCs) in pigs after myocardial infarction. Cells were labeled 90 minutes before injection with 100 MBq of $^{125}$I and a volume of 250 μL was injected in three regions of the animals' hearts. The anterior wall of the left ventricle received 50 million cells of human MSCs. The lateral and septal walls received 50 million NIS-positive [NIS(pos)] human iPSCs or 50 million NIS(pos) human iPSCs mixed with 50 million human MSCs. $^{99m}$Tc-tetrofosmin was intravenously injected to assess myocardial perfusion. Images were acquired for 5 minutes in SPECT/CT equipment. Images were acquired up to 15 weeks after cell transplantation through an intracoronary injection of $^{125}$I. No uptake was seen outside the heart and NIS(pos) human iPSCs were detected in the site of injections, indicating successful cell homing.

Yan et al. [63] assessed the distribution of BM-MSCs in nude mice 10 minutes after induction of myocardial infarction. Cells transfected with a TK gene were injected intramyocardially after induction of the lesion. On the same day and 3 and 7 days after cell transplantation, $^{18}$F-FBG was injected and PET was carried out. The authors described that the highest myocardial uptake occurred 3 days after cell therapy and that infarcted animals had higher homing than control animals.

Pei et al. [64] evaluated the homing of BM-MSCs in rats after myocardial infarction. Immediately after the lesion, cells were intramyocardially injected. Two, 3, and 7 days after cell transplantation, $^{18}$F-FHBG was injected to allow cell tracking. The authors reported that myocardial uptake could be seen up to 7 days following cell therapy, and homing was mostly distributed to the liver, lungs, intestines, stomach, and spleen.

Lee et al. [65] studied the distribution of ADSCs transfected with the NIS gene in dogs following myocardial infarction. NIS expressing ADSCs were intramyocardially injected 7 days after the infarct induction. $^{99m}$TcO4- was injected at 2 hours and 1, 2, 5, 7, 9, and 12 days after cell transplantation. The authors reported that cell homing was identified in the apex and lateral wall of the left ventricle, reached its peak at 2 days, and was seen until 9 days after cell transplantation.

4. Clinical Trials

4.1. Direct Cell Labeling. We have found 18 published articles in English regarding 17 different trials that employed radionuclides to track cell therapies for cardiac diseases, with a total of 293 treated patients (Table 3). All studies used direct labeling methods.

4.1.1. Biodistribution after Intracoronary Injection. Cavilers et al. [66] conducted a cell therapy trial with eight chronic ischemic heart disease patients. They reported that infusion of CD133+ selected PB-MNCs labeled with $^{111}$In-oxine is a safe and feasible procedure. They also performed $^{99m}$Tc-MIBI SPECT for evaluation of myocardial perfusion and compared it to cell migration. Uptake in the heart was 6.9% to 8% and 2.3% to 3.2% after 2 and 12 hours, respectively.

Kurpisz et al. [67] studied the migration of BM-MNCs in 3 patients with acute myocardial infarction. Cells were labeled with $^{111}$In-oxine and injected by intracoronary route. Nuclear Medicine imaging was carried out 24 hours after cell transplantation. The authors reported that 2.6–11.0% of the uptake was seen in the heart, 12.3–56.7% in the liver, and 5.2–12.6% in the spleen.

Schots et al. [68] evaluated 13 patients with nonacute myocardial infarction who received CD133+ cells labeled with $^{111}$In-oxine by intracoronary transplantation. Subjects had uptake of 6.9 to 8.0% in the myocardium in 2-hour images and 2.3 to 3.2% in 12-hour images.

Schächinger et al. [69] included 20 patients with ischemic myocardial disease that had myocardial viability confirmed by PET and intracoronary Doppler. The time of coronary injury to BM-MNC therapy ranged from 5 days to 17 years. After administration of $^{18}$F-FDG labeled cells, the average myocardial uptake in the first 24 hours was higher in subjects with acute myocardial infarction and gradually decreased
Table 3: Clinical studies that used direct radiopharmaceutical labeling for cell therapies in cardiology.

<table>
<thead>
<tr>
<th>Study reference</th>
<th>Radiopharmaceutical</th>
<th>Type of lesion</th>
<th>Cell type</th>
<th>Route</th>
<th>Number of patients</th>
<th>Number of cells injected</th>
<th>Imaging time points</th>
</tr>
</thead>
<tbody>
<tr>
<td>Hofmann et al., 2005</td>
<td>^18^F-FDG</td>
<td>Acute myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>12</td>
<td>Not specified</td>
<td>75 min</td>
</tr>
<tr>
<td>Blocklet et al., 2006</td>
<td>^111^In-oxine</td>
<td>Acute myocardial infarction</td>
<td>PB-MNCs</td>
<td>Intracoronary</td>
<td>6</td>
<td>2–4 × 10^6</td>
<td>1 hour (^18^F-FDG) 19 and 43 hours (^111^In-oxine)</td>
</tr>
<tr>
<td>Kang et al., 2006</td>
<td>^18^F-FDG</td>
<td>Acute or nonacute myocardial infarction</td>
<td>PB-MNCs</td>
<td>Intracoronary</td>
<td>20</td>
<td>Not specified</td>
<td>2, 4, and 20 hours</td>
</tr>
<tr>
<td>Goussis et al., 2006</td>
<td>^99m^Tc-HMPAO</td>
<td>Chronic ischemic cardiomyopathy</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>8</td>
<td>0.8 × 10^7</td>
<td>1 and 24 hours</td>
</tr>
<tr>
<td>Caveliers et al., 2007</td>
<td>^111^In-oxine</td>
<td>Chronic ischemic cardiomyopathy</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>8</td>
<td>5–35 × 10^6</td>
<td>2 and 12 hours</td>
</tr>
<tr>
<td>Penicka et al., 2007</td>
<td>^99m^Tc-HMPAO</td>
<td>Acute or nonacute myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>10</td>
<td>24.2–57.0 × 10^8</td>
<td>2 and 20 hours</td>
</tr>
<tr>
<td>Kurpise et al., 2007</td>
<td>^111^In-oxine</td>
<td>Acute myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>3</td>
<td>2–4 × 10^6</td>
<td>24 hours</td>
</tr>
<tr>
<td>Schots et al., 2007</td>
<td>^111^In-oxine</td>
<td>Nonacute myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>8</td>
<td>5–10 × 10^6</td>
<td>2 and 12 hours</td>
</tr>
<tr>
<td>Schächiger et al., 2008</td>
<td>^111^In-oxine</td>
<td>Acute or nonacute myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>20</td>
<td>15 × 10^6</td>
<td>1 and 24 hours</td>
</tr>
<tr>
<td>Dedobbeleer et al., 2009</td>
<td>^18^F-FDG</td>
<td>Acute myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>7</td>
<td>1.8 × 10^7</td>
<td>1 hour</td>
</tr>
<tr>
<td>Silva et al., 2009;</td>
<td>^99m^Tc-HMPAO</td>
<td>Acute myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>30</td>
<td>1 × 10^7</td>
<td>4 and 24 hours</td>
</tr>
<tr>
<td>Moreira et al., 2011</td>
<td>^99m^Tc-HMPAO</td>
<td>Acute myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>34</td>
<td>0.92–7.54 × 10^6</td>
<td>1 hour</td>
</tr>
<tr>
<td>Barbosa da Fonseca et al., 2011</td>
<td>^99m^Tc</td>
<td>Acute myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>6</td>
<td>4.4 × 10^8</td>
<td>1, 3, and 24 hours</td>
</tr>
<tr>
<td>Kollaros et al., 2012</td>
<td>^99m^Tc-HMPAO</td>
<td>Chronic chagasic cardiomyopathy</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>13</td>
<td>Not specified</td>
<td>1 hour</td>
</tr>
<tr>
<td>Musialek et al., 2011</td>
<td>^99m^Tc-HMPAO</td>
<td>Acute myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>31</td>
<td>4.3 × 10^6</td>
<td>1 hour</td>
</tr>
<tr>
<td>Barbosa da Fonseca et al., 2011</td>
<td>^99m^Tc</td>
<td>Recent myocardial infarction</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>3</td>
<td>1 × 10^6</td>
<td>18 hours</td>
</tr>
<tr>
<td>Vrtovec et al., 2013</td>
<td>^99m^Tc-HMPAO</td>
<td>Nonischemic dilated cardiomyopathy</td>
<td>BM-MNCs</td>
<td>Intracoronary</td>
<td>40</td>
<td>1 × 10^6</td>
<td>18 hours</td>
</tr>
<tr>
<td>Haddad et al., 2015</td>
<td>^99m^Tc-HMPAO</td>
<td>Nonischemic dilated cardiomyopathy</td>
<td>PB-MNCs</td>
<td>Transendocardial</td>
<td>37</td>
<td>75 × 10^6</td>
<td>2 and 18 hours</td>
</tr>
</tbody>
</table>

^111^In: indium-111; ^18^F: fluorine-18; ^99m^Tc: technetium-99m; BM-MNCs: bone marrow mononuclear cells; FDG: fluorodeoxyglucose; HMPAO: hexamethylpropyleneamine oxime; IRCV: interstitial retrograde coronary venous; PB-MNCs: peripheral blood mononuclear cells.
in subjects treated in an intermediate or chronic phase. The authors concluded that the low viability of the lesioned myocardium and the reduction of coronary flow reserve were important predictors in the proangiogenic potential of progenitor cells.

Dedobbeleer et al. [70] published a study of 12 patients with nonacute myocardial infarction. Five patients were in the control group and 7 patients had CD34+ cells labeled with 18F-FDG. After an hour of injection, 3.2% of the radioactivity was observed in the myocardial infarction zone.

Blocklet et al. [71] evaluated the injection of PB-MNCs labeled with 111In-oxine and 18F-FDG in 6 patients with acute myocardial infarction. The double labeling allowed monitoring of cell with high sensitivity and resolution with PET and performing late images with 111In. Mean uptake in the myocardium after 1-hour infusion of PB-MNCs was 5.5% by PET, while in images with 111In-oxine at 19 hours and 43 hours only 1 patient had myocardial uptake.

4.1.2. Comparison of Biodistribution of Intracoronary and Intravenous Injection. Hofmann et al. [72] carried out a cell therapy trial 5 to 10 days after a myocardial infarction in 9 patients using CD34+ BM-MNCs. Of the total amount of injected cells, 5% were labeled with 18F-FDG. The patients were divided into 3 protocols. In the first protocol, 3 patients received unselected BM-MNCs by intracoronary route and underwent PET imaging 55 to 75 minutes after infusion. In a second protocol, 3 patients initially received 5% of the unselected BM-MNCs by intravenous route, followed by a first PET 50 to 60 minutes after cell transplantation, and then received the remaining 95% of unselected BM-MNCs by intracoronary route, followed by a second PET 60 to 70 minutes later. In a third protocol, 3 patients received immunomagnetically enriched CD34+ cells by intracoronary route and underwent PET imaging 60 to 75 minutes after cell injection. In the first protocol, homing varied from 1.3% to 2.6%. In the second group, there was no detectable myocardial homing after the initial intravenous infusion, but homing increased to 1.8 to 5.3% after intracoronary injection. In the third group, in which CD34+ cells were injected by intracoronary route, cell homing was higher, ranging from 14% to 39%.

Kang et al. [73] published a report in which 20 patients with recent or old myocardial infarctions received PB-MNCs labeled with 18F-FDG. The PB-MNCs were collected by apheresis after mobilization with granulocyte colony stimulating factor (G-CSF). Seventeen of the patients received cells by intracoronary route and 3 patients by intravenous route. The mean efficiency of cell labeling with 18F-FDG was of 72% and a total activity of 44.4 to 175 MBq was injected through a catheter after stent implantation in the infarcted artery. PET/CT images were obtained 2, 4, and 24 hours after injection. Two hours after intracoronary injection, 1.5% of the infused cells were present at the lesioned area. Delayed images up to 20 hours indicated prolonged accumulation of the cells in heart tissue. Intravenous infusion of the labeled PB-MNCs revealed high pulmonary trapping and showed no significant activity in the heart.

Goussetis et al. [74] studied 8 subjects with chronic ischemic heart disease undergoing CD133+ and CD133−CD34+ selected BM-MNC transplantation by intracoronary infusion. Cells were labeled with 99mTc and scintigraphies acquired 1 and 24 hours after injection indicated cardiac uptake of 9.2% and 6.8%, respectively. Reevaluation with coronary angiography and echocardiography in 6 patients after 3 months of cell therapy revealed no complications.

Penicka et al. [75] included 10 patients, 5 of them with acute myocardial infarction and the other 5 with nonacute myocardial infarction. All patients received BM-MNCs labeled with 99mTc-HMPAO and myocardial uptake was analyzed 2 and 20 hours after injection. There was a lack of uptake 20 hours after transplantation in subjects with acute myocardial infarction.

A randomized study of 30 subjects with acute myocardial infarction, published by Silva et al. [76] and Moreira et al. [77], compared the distribution and retention pattern of 99mTc-HMPAO labeled BM-MNCs after anterograde intrarterial or retrograde intravenous coronary routes. The early and late retention of labeled cells, evaluated in 4 and 24 hours SPECT images after injection, were higher in the group that received cells by coronary anterograde, regardless of the presence of microcirculation obstruction. Early and late retention were, respectively, 7.06% and 6.38% in the intraarterial group and 1.4% and 0.99% in the intravenous group.

Musialek et al. [78] compared the cell transplant management techniques: perfusion technique catheter (PC) and the over-the-wire coronary occlusion technique (OTW). Thirty-four patients who suffered myocardial infarction were randomly assigned to PC or OTW infusion of autologous bone marrow CD34+ cells labeled with 99mTc-HMPAO. One hour after infusion, the images obtained by SPECT indicated the activity of 4.86% and 5.05% in the myocardium after OTW and PC injections, respectively. The authors concluded that although the efficacy of cell delivery did not differ between infusion methods, PC infusion offered a more physiological alternative and avoided causing OTW ischemic episodes. The same group performed another study evaluating the migration of intracoronary injected 99mTc-HMPAO labeled bone marrow CD34+ cells in subjects after myocardial infarction. The authors described that, one hour after cell transplantation, mean cardiac uptake was 5.2% [79].

Our group published a study with 6 Chagasic cardiomyopathy patients who received intracoronary injection of 99mTc labeled BM-MNCs [80]. SPECT images performed 1, 3, and 24 hours after administration of the labeled cells revealed a myocardial uptake of 5.4%, 4.3%, and 2.3%, respectively. Such decrease in relative myocardial uptake could be related to leakage of 99mTc from labeled cells and not to a reduction in the number of cells. We also observed that the cell distribution was heterogeneous and limited and was related with the pattern of myocardial perfusion.

Kollaros et al. [81] compared images obtained from the perfusion study with 201Tl and images after intracoronary infusion of BM-MNCs labeled with 99mTc-HMPAO. In the thirteen patients, images were complementary and revealed accurate localization of cells in the lesioned area. There was
intense cell accumulation in areas without viability as evaluated by $^{201}$Tl scintigraphy. The percentage (83.2%, ranging from 56.4 to 97.2%) of the infarcted area that had retained cells was determined by merging $^{99m}$Tc and $^{201}$Tl images.

4.1.3. Comparison of Biodistribution after Intracoronary and Transendocardial Cardiac Injection. Vrtovec et al. [82] included a total of 40 patients, where 20 received $^{99m}$Tc labeled BM-MNCs by intracoronary and another 20 by transendocardial route. The relative uptake after 18 hours after injection was 4.4% and 19.2% in intracoronary and transendocardial routes, respectively.

Haddad et al. [83] included thirty-seven patients with nonischemic dilated cardiomyopathy. On average, $75 \times 10^6$ CD34$^+$ PB-MNCs were labeled with $^{99m}$Tc-HMPAO and infused via transendocardial route. SPECT images were acquired 2 and 18 hours after infusion to assess the homing and cellular distribution as well as detect cell migration potential. Twenty-eight patients consented to further myocardial homing imaging. In those patients, the stem cells homing rate had a median value of 11.4% (range 3.8%–22.3%).

5. Alternative Approaches to Cell Tracking

Besides radionuclide labeling, different techniques may be used to study cell distribution in vivo. Fluorescence imaging (FLI) and bioluminescence imaging (BLI) have been effectively employed to track cells in preclinical studies of cell transplantation for cardiac diseases [84, 85]. Nevertheless, factors such as the limited tissue penetration of light hinder the clinical application of FLI and BLI [86]. Superparamagnetic iron oxide nanoparticles (SPIONs), originally created to detect liver tumors in patients after intravenous infusion, were adapted for preclinical exogenous cell labeling, which allowed the study of cell migration for weeks following transplantation with exceptional resolution and morphologic correspondence with MRI [87]. Early clinical studies have been conducted in studies of cell therapies for noncardiac diseases [88–92]. Nonetheless, SPION labeling has restrictions of other exogenous contrasts, for instance, the possibility of dilution with cellular division and of stem cell phagocytosis by macrophages. Moreover, there are differing data on the burden of nanoparticle cell labeling in biological properties [93–96], and exogenous SPION cell labeling has only been approved for research applications.

Due to these factors, radiopharmaceutical labeling continues to be a relevant technique for the assessment of stem cell distribution in vivo [7]. It allows more accurate definition of cell location and the combination of Nuclear Medicine with CT or MRI enables the study of diverse characteristics, for example, (1) comparison of cell migration with structural and functional results and (2) the outcome of different cell doses and injection methods on cell homing.

6. Impact of the Route of Administration

Radiopharmaceutical cell tracking has already increased understanding of cell migration in preclinical and clinical studies of cell therapies for cardiac diseases. Among other conclusions, preclinical [55] and clinical [54, 73] studies indicated that intravenous infusions of BM-MNCs and PB-MNCs lead to lower cardiac homing in comparison with intracoronary injections. On the other hand, intramyocardial injection of PB-MNCs [97] and BM-MNCs [53, 54] led to greater cardiac homing of transplanted cells in comparison to intracoronary infusion in preclinical studies. Similarly, transendocardial injection of BM-MNCs led to greater homing in comparison to intracoronary infusion in subjects with nonischemic dilated cardiomyopathy [82].

Even though there have been preclinical and clinical studies investigating the potential of MSC transplantation for cardiac diseases, to our knowledge, no clinical studies yet have tracked MSC migration with noninvasive imaging. Moreover, clinical trials of radiopharmaceutical cell tracking remain restricted to PB-MNC and BM-MNC trials.

Nevertheless, it is still unclear if more intense myocardial homing is important to improve the outcome of cell therapies for cardiac diseases. Different groups have suggested that, instead of differentiation into cardiac cells, the mechanisms of stem cell therapies may be at least partially due to interactions between injected and host cells, such as the secretion of trophic factors [98]. For example, BM-MSCs may assume distinctive phenotypes after receiving stimuli from proinflammatory cytokines or when submitted to a hypoxic milieu in vitro [98].

As previously mentioned, intravenously injected stem cells may suffer pulmonary entrapment [99]. The lungs may characterize an obstacle for cell migration [99] but might also be essential for the triggering of stem cell responses, before their homing to the heart. Lee et al. [100] reported that an increased production of the tumor necrosis factor inducible gene 6 protein (TGS-6) in BM-MSCs is entrapped in the lungs after intravenous injection in mice following acute myocardial infarction. Their report suggested that BM-MSCs were stimulated in the lungs to produce TGS-6, which controlled myocardial inflammatory response.

7. Conclusion

Methods for cell tracking with radioisotopes are feasible and efficient and different studies have used it to monitor migration in cell therapies for cardiac diseases. These techniques provide validated quantifications of cell retention in different organs and the dynamics of cell distribution in the whole body. However, additional reports are needed to increase the knowledge of the mechanisms responsible for cell migration and homing and their relationship with possible structural and functional outcomes of cell transplantation for cardiac diseases.

Conflict of Interests

The authors declare that there is no conflict of interests regarding the publication of this paper.
Authors’ Contribution

Mayra Lorena Moreira and Priscylla da Costa Medeiros contributed equally to this work and should be considered co-first authors.

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