

Research Article

Preparation and Characterization of Self-Emulsified Docetaxel

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The aim of this paper was to prepare a self-microemulsifying docetaxel (Dtx) using PLGA, Tetraglycol, Labrasol, and Cremophor ELP. The prepared Dtx-loaded self-microemulsifying system (SMES) showed the initial size of the range of 80–100 nm with narrow size distribution and the negative zeta-potential values. Its morphology was a spherical shape by atomic force microscopy. In experiment of stability, Dtx-loaded SMES prepared in DW and BSA condition showed good stability at 37°C for 7 days. The viability of the B16F10 cells incubated with Dtx-loaded SMES, Dtx-solution, and Taxol were decreased as a function of incubation time. In conclusion, we confirmed that Dtx-loaded SMES showed an inhibitory effect for proliferation of B16F10 melanoma cells.

1. Introduction

The first-line treatment of various cancers includes surgery, radiotherapy, or a combined treatment regimen [1–4]. As second-line treatment for cancer, the chemotherapy using anticancer drugs may be treated to remove completely cancers [1–6]. Many highly potent anticancer drugs are clinically treated as available commercial products. However, the utility of these cancer chemotherapeutic drugs in clinical applications is limited by very low solubility in aqueous [7, 8].

Paclitaxel (Ptx), isolated from the bark of *Taxus brevifolia*, has significant activity against a variety of tumors such as breast cancer, advanced ovarian carcinoma, lung cancer, and head and neck carcinoma [9]. Docetaxel (Dtx) is also an anticancer drug belonging to the second generation of the taxoid family [10]. Ptx and Dtx are hydrophobic drugs with poor aqueous solubility [11, 12]. To enhance solubility of Ptx, it is currently formulated for clinical application as Taxol by Cremophor EL-based solvent system containing dehydrated ethanol [13].

Recently, various formulations such as liposomes, emulsions, micelles, microspheres, and polymeric nanoparticles have been employed for the encapsulating Ptx and Dtx including several anticancer drugs [14–20]. The selection of

a proper Ptx and Dtx encapsulating formulation is important to improve the instability problems such as subsequent precipitation of the solubilised hydrophobic Ptx and Dtx for in vivo treatment.

The poor water solubility of Ptx and Dtx can be improved by the formulation with oil, low molecular weight surfactants, and so forth. The self-microemulsifying system (SMES) are isotropic mixtures of oil, a surfactant, and cosurfactants, which form fine oil-in-water emulsions when exposed to aqueous media [21–23]. Thus, the SMES was found to be highly suitable for the incorporation of hydrophobic Ptx and Dtx. Because SMES may be a promising way to load hydrophobic Dtx in delivery system, here, we report on the preparation of Dtx-loaded SMES which could result in an improvement of stability of the solubilised hydrophobic Dtx in aqueous media.

2. Materials and Methods

2.1. Materials. Poly (d,l-lactide-co-glycolide) (PLGA, molecular weight, 8,000, 20,000 and 90,000 g/mole) was purchased from Boehringer Ingelheim (Ingelheim, Germany). Docetaxel was purchased from Naprod Life Science Pvt, Ltd (India). Paclitaxel (Genexol) was purchased from Samyang

TABLE 1: Formulation for the preparation of Dtx-loaded SMES.

Composition (g, w/w)	Formulation		
	F1	F2	F3
Drug (Docetaxel)		0.003	
Solubilizer (Tetraglycol)		0.5	
PLGA 8k g/mol	0.005		
PLGA 20k g/mol		0.005	
PLGA 90k g/mol			0.005
Cosurfactant (Labrasol)		0.14	
Surfactant (Cremophor ELP)		0.16	
Zeta-potential (mV)	-7.7 ± 0.4	-2.8 ± 1.3	-4.3 ± 0.6

Genex Co. (Seoul, Korea). Caprylocaproyl macrogol-8 glyceride (Labrasol) was obtained from Gattefosse (Westwood, NJ, USA). Cremophor ELP was purchased from BASF (Germany). Tetraglycol was purchased from Sigma Chemical Co. (St. Louis, MO, USA). All other chemicals were of reagent grade. The deionized water (DW) was prepared by a Milli-Q purification system from Millipore (Molsheim, France).

2.2. Preparation of Dtx-Loaded SMES, Dtx-Solution, and Taxol. A series of SMES was prepared in each of the various formulas with PLGA, docetaxel, solubilizer, surfactant, and cosurfactant. Briefly, PLGA, Dtx, Tetraglycol, Labrasol, and Cremophor ELP in the various ratios (Table 1) were added into the vial, followed by heating on a hot plate to 60–70°C with stirring and vortex mixing until Dtx had perfectly dissolved. A solution of 3 mg of SMES was carefully weighed in 10 mL tube. It was then emulsified by contacting to 7 mL DW and vortexed, followed by keeping at room temperature for about 30 minutes to use in subsequent studies. The prepared Dtx-loaded SMES used without any purification. A 6 mg of Dtx and Ptx was added into 10 mL mixture of Cremophor EL and ethanol (v/v = 1/1) to prepare Dtx-solution and Taxol, respectively [19–21].

2.3. Dtx Encapsulation Efficiency. The Dtx-loaded SMES and Dtx-solution prepared as final concentration of 0.43 mg/mL of Dtx in 7 mL DW. The flask was allowed to equilibrate for 30 minutes at RT. The solution was thereafter filtered through a filter paper. The Dtx encapsulation efficiency in the solution was analyzed using a high-performance liquid chromatography (HPLC), Agilent 1200 series LC system equipped with detection at 220 nm using a diode array detector (Agilent Technologies, Inc., Santa Clara, USA). A Sunfire C18 column (4.6 × 150 mm, 5 μm) was used. The mobile phase consisted of a distilled water:acetonitrile:methanol (41:48:11 v/v) mixture, and the column was eluted at a flow rate of 1.0 mL/min. The Dtx encapsulation efficiency was calculated by comparison with the standard calibration curves prepared with known concentrations of Dtx. Three

independent Dtx-loaded SMES experiments were performed for each Dtx encapsulation efficiency and then averaged.

2.4. Size Analysis of Dtx-Loaded SMES, Dtx-Solution and Taxol. For analysis, formulation (50 μL) of Dtx-loaded SMES, Dtx-solution and Taxol were diluted with 50 mL DW in volumetric flask, followed by vortex mixing gently mixed. The particle size, size distribution, and surface charge of resultant formulation were determined by dynamic light scattering (DLS, ELS-8000, Photol, Japan) at room temperature. The analysis was individually measured for three samples of Dtx-loaded SMES, Dtx-solution, and Taxol, and then calculated as average value using three individual sizes.

2.5. Morphology of Dtx-Loaded SMES. The shape and surface morphology were investigated by atomic force microscopy (AFM). A 10 μL of Dtx-loaded SMES was transferred onto silicon wafer which was washed with MeOH. The wafer was quickly placed in liquid nitrogen, followed by the freeze-drying for 2 days. AFM measurements were carried out in the tapping mode with a nanoscope IV instrument (Digital Instruments Inc.).

2.6. Stability of Dtx-Loaded SMES, Dtx-Solution, and Taxol. Dtx-loaded SMES, Dtx-solution, and Taxol were prepared with 7 mL DW or a solution of 0.9% NaCl and 5% bovine serum albumin (Bovogen, Australia) and individually placed in 10 mL tube. The tube was constantly shaken at 100 rpm and 37°C for 7 days. At the set time, the droplet size was individually measured for three samples of Dtx-loaded SMES, Dtx-solution, and Taxol, and then calculated as average value.

2.7. Cell Culture. B16F10 melanoma cell line was obtained by Korea Cell Line Bank and cultured in culture media (MEM (Minimum Essential Medium, Gibco BRL, USA) supplemented with 10% fetal bovine serum (Gibco BRL, USA) and 1% PS (Penicillin streptomycin, Gibco BRL, USA)), and maintained at 37°C in 5% CO₂ humidified atmosphere. The cells were seeded into 75-cm² flasks, cultured, and changed medium every 2 days.

2.8. Cell Cytotoxicity Tests. B16F10 cell suspension (2 × 10⁴ cells/well) was seeded in a 48-well plate. The cells were incubated overnight to allow for cell attachment under culture media. The cells were incubated without and with Dtx-loaded SMES, Dtx-solution, and Taxol for 7 days without changing of culture media [19–21]. The final concentration of the Dtx and Ptx in the cell culture medium was adjusted to 1 μg/mL. Cell viability was determined by using water-soluble enzyme substrate MTT which was converted to purple water-insoluble product formazan accumulated in the cytoplasm of viable cells. Cell viability of each well performed individually and then calculated as average value. In brief, 100 μL of PBS solution of the MTT tetrazolium substrate (5 mg/mL) was added after 1, 4, and 7 days. After incubation for 4 h at 37°C, the resulting purple formazan precipitate was solubilized by the addition of 1 mL of DMSO and shaken

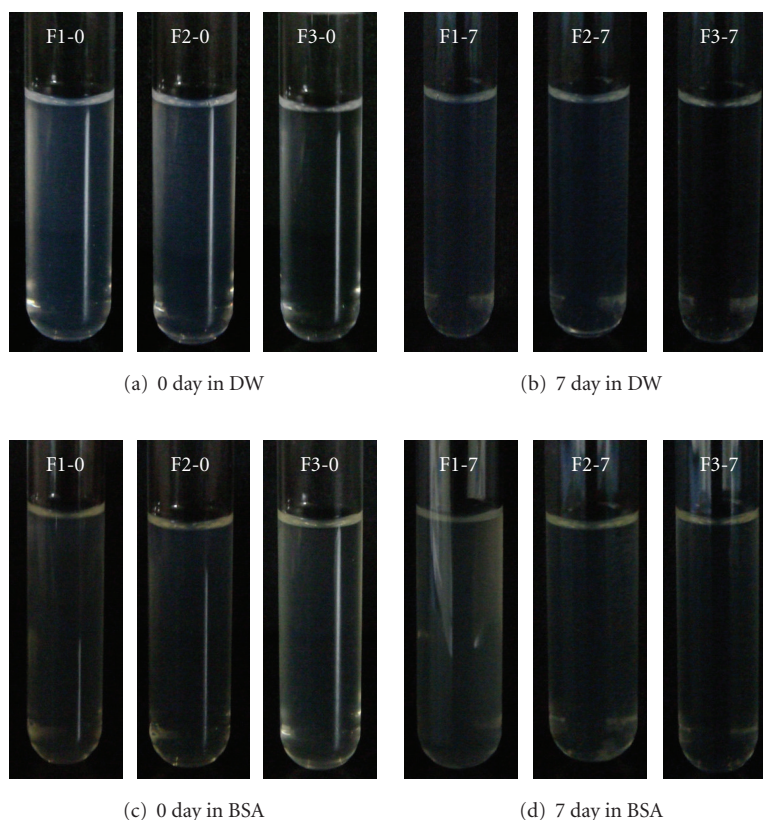


FIGURE 1: Pictures (a, c) before and (b, d) after incubation at 37°C for 7 days of Dtx-loaded SMES prepared in (a, b) DW and (c, d) BSA with different formulations F1–F3.

for 30 minutes. An aliquot from each well (100 μ L) was transferred to 96-well plates and then read using a plate reader of an ELISA (E-max, Molecular Device, USA). The optical density of each well was determined at 590 nm.

2.9. Statistical Analysis. Cytotoxicity data were obtained from independent experiments in which each of the five treatment conditions were tested in triplicate. All data are presented as means \pm standard deviations (SD). The results were analyzed by one-way ANOVAs using the Prism 3.0 software package (GraphPad Software Inc., San Diego, CA, USA).

3. Results and Discussion

3.1. Preparation of Dtx-Loaded SMES. The Dtx-loaded SMES were prepared by using Dtx, tetraglycol, Cremophor ELP, Labrasol, and PLGA; the formulation is summarized in Table 1. The prepared Dtx-loaded SMES were observed visually. As shown in Figure 1(a) Dtx-loaded SMES (F1–F3) showed the transparent emulsion solution for all formulations, indicating that Dtx was successfully incorporated into the SMES. The Dtx encapsulation efficiency is above 70%. Dtx-solution and Taxol showed the transparent solution.

The size and size distribution of Dtx-loaded SMES measured by DLS were shown in Table 2. The average size

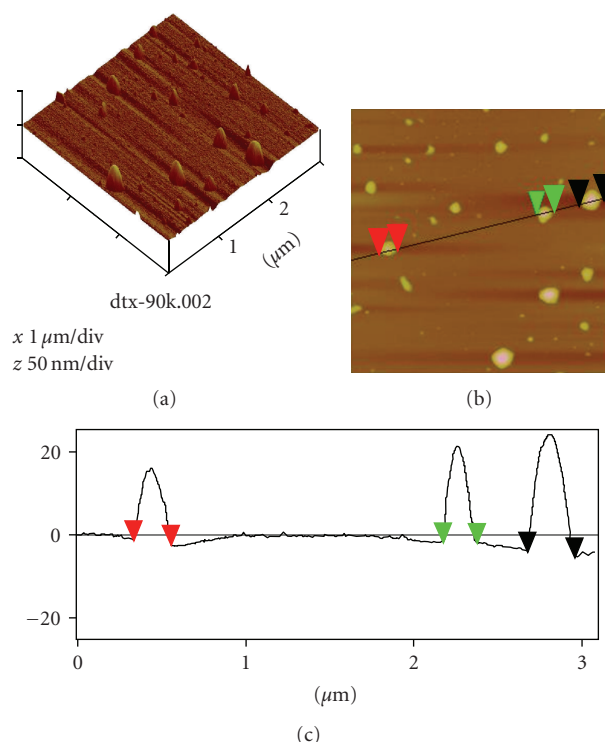


FIGURE 2: AFM image of Dtx-loaded SMES (F3).

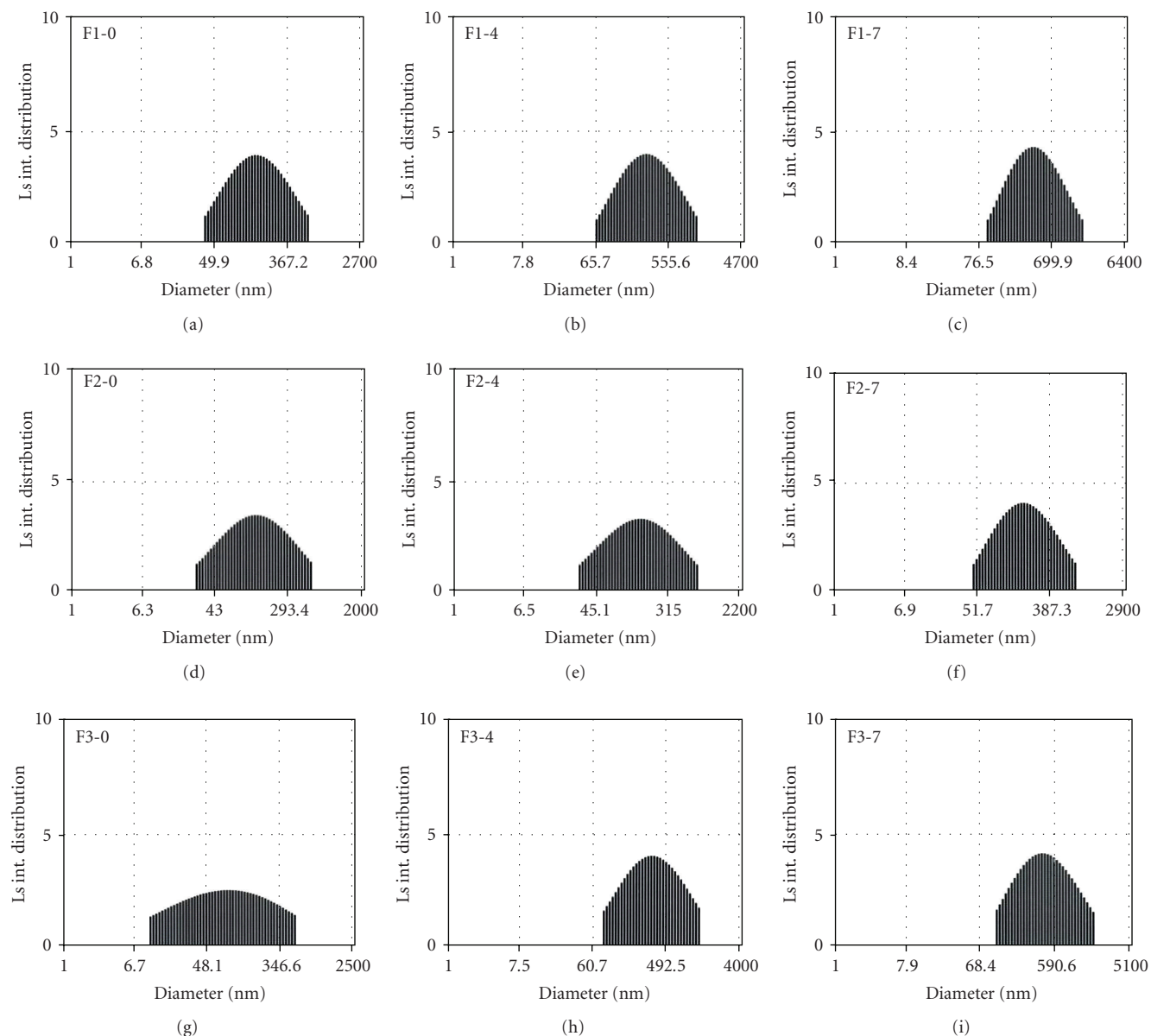


FIGURE 3: DLS images measured after incubation at 37°C at 0, 4, and 7 days of Dtx-loaded SMES prepared in BSA with different formulations F1–F3 (0, 4 and 7 represent the incubation time).

of the Dtx-loaded SMES determined from the DLS was in the range of 80–100 nm. It seemed that the changes of PLGA molecular weight did not significantly affect the size of the resultant Dtx-loaded SMES. Even though the droplet size distribution was slightly broader for increasing PLGA molecular weight, F1–F3 is formulation with appropriate size. Meanwhile, Dtx-solution and Taxol showed the average size in the range of 200–300 nm.

The AFM morphology of Dtx-loaded SMES showed the spherical shape with smooth surface as shown in Figure 2. A comparatively uniform droplet size of Dtx-loaded SMES was also observed at AFM, indicating no aggregation or adhesion among SMES.

3.2. Stability of Dtx-Loaded SMES. The stability of Dtx-loaded SMES is important to maintain the in vivo therapeutic concentration of Dtx. Surface charge may be an important indication for the stability of Dtx-loaded SMES in medium. The zeta potential of the Dtx-loaded SMES indicates the negative surface charges (Table 1). This implies that the repulsion among the Dtx-loaded SMES with the same type of surface charge can provide stability.

To examine stability of the solubilised Dtx in DW and BSA condition, Dtx-loaded SMES, Dtx-solution, and Taxol were prepared with DW or a solution of 0.9% NaCl and 5% BSA (Figures 1 and 4). The prepared Dtx-loaded SMES, Dtx-solution, and Taxol were constantly shaken at 100 rpm and

TABLE 2: The changes of average particle size by incubation for 0–7 days at 37°C of Dtx-loaded SMES prepared in DW and BSA condition with different formulations F1–F3.

Condition		In DW			In BSA condition ^a		
Formulation		F1	F2	F3	F1	F2	F3
Particle size (nm) ^b	Initial	85 ± 1	92 ± 3	93 ± 13	116 ± 4	87 ± 2	113 ± 8
	4 days	93 ± 5	88 ± 4	77 ± 20	218 ± 15	93 ± 6	167 ± 11
	7 days	115 ± 5	99 ± 4	93 ± 15	234 ± 3	126 ± 9	226 ± 3

^aA solution of 0.9% NaCl and 5% bovine serum albumin.

^bThe mean and standard deviation of particle size for each formulation was calculated by individual measurement of three formulations.

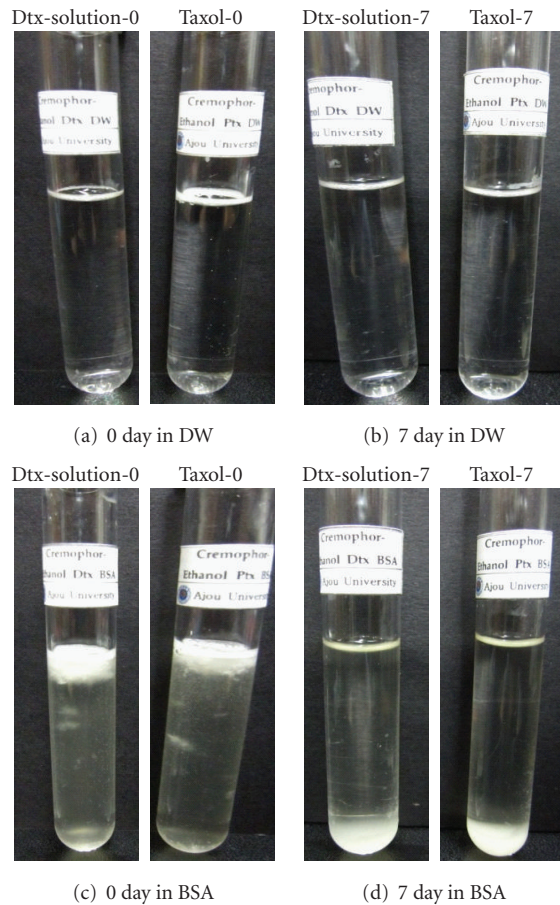


FIGURE 4: Pictures (a, c) before and (b, d) after incubation at 37°C for 7 days of Dtx-solution and Taxol prepared in (a, b) DW and (c, d) BSA.

37°C for 7 days. There is a little change of particle size for F1–F3, Dtx-solution, and Taxol prepared in DW as shown in Figures 1(b) and 1(d), indicating the stability of Dtx-loaded SMES, Dtx-solution, and Taxol in DW.

For Dtx-loaded SMES, Dtx-solution, and Taxol prepared in BSA, the size of Dtx-loaded SMES steadily increased as a function of time (Table 2). The sizes of F1 and F3 at 7 days were approximately two times larger than those at 0 day. Meanwhile, F2 was maintained the original size for at least 4 days and only increased from 87 to 126 nm (Figure 3). It can be noted that proper Dtx encapsulating formulation can lead to stability of solubilised Dtx. Meanwhile Dtx-solution and

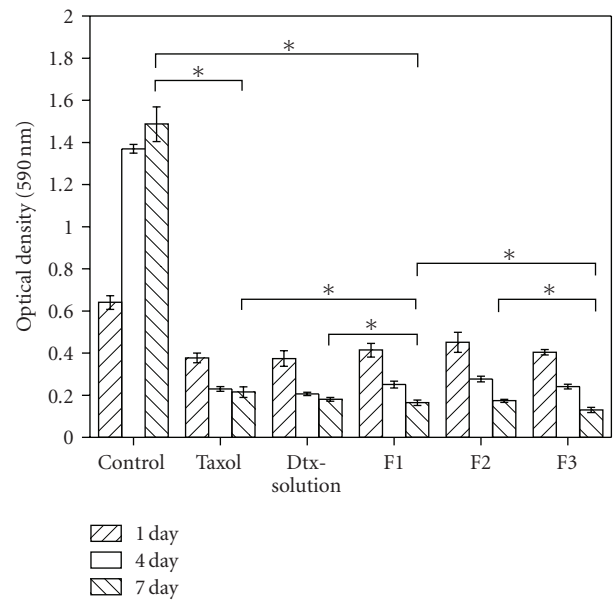


FIGURE 5: In vitro cytotoxicity of B16F10 melanoma cell against Dtx-loaded SMES of formulations F1, F2, and F3 for 1, 4, and 7 days. The cells grown on a culture plate without Dtx-loaded SMES were used as the control and the cells with Taxol and Dtx-solution were used for comparison (* $P < .001$).

Taxol precipitated immediately in BSA condition, indicating nonstability of Dtx-solution and Taxol (Figure 4).

3.3. Antitumor Activity of Dtx-Loaded SMES. The cytotoxicity for Dtx-loaded SMES (F1–F3), Dtx-solution, and Taxol for comparison was evaluated using B16F10 melanoma cell line (Figure 5). The B16F10 cells in the control experiment proliferated as a function of culture time. However, the viability of the B16F10 cells incubated with Dtx-loaded SMES (F1–F3) was approximately 50%–60% and 30%–40% at 4 days and 7 days, indicating that increasing the incubation time from 24 to 48 h led to more cell death. A similar viability of the B16F10 cells was observed when Dtx-solution and Taxol were used for 4 days. However, the viability of the B16F10 cells for Dtx-solution and Taxol was maintained when the incubation time was extended to 7 days. This indicates that the Dtx-loaded SMES was somewhat more effective in inhibition of B16F10 cell proliferation than Dtx-solution and Taxol. Thus, it appeared that the slightly

improved inhibition of B16F10 cell proliferation may be due to the Dtx-loaded SMES's stability.

4. Conclusion

The authors prepared the Dtx-loaded SMES to improve their stability. The prepared Dtx-loaded SMES showed a spherical shape in the range of 80–90 nm. The authors found that the formulation of the Dtx-loaded SMES prepared in DW and BSA showed a little change in the particle size for 7 days. Dtx-loaded SMES showed an inhibitory effect on B16F10 melanoma proliferation. Thus, further research on the animal model using Dtx-loaded SMES prepared in this work is now in progress.

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