Noninvasive Evaluation of EGFR Expression of Digestive Tumors Using $^{99m}$Tc-MAG$_3$-Cet-F(ab′)$_2$-Based SPECT/CT Imaging

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1. Introduction

Gastric cancer and colon cancer are common digestive system tumors, with incidence rates ranked fifth [1] and third [2] among that of all tumors, respectively. Gastric cancer and colon cancer are both among the top five causes of tumor-related death. Many patients are already at the advanced stages when diagnosed and are therefore usually unsuitable for radical surgery. Advances in the assessment of the target point in targeted therapy have contributed to increased treatment effectiveness and improved survival of patients with cancer over the past decades. Epidermal...
growth factor receptor (EGFR), the receptor for EGF cell proliferation and signal transduction, is related to the inhibition of tumor cell proliferation, angiogenesis, tumor invasion, metastasis, and apoptosis [3, 4]. Monoclonal antibody (mAb) treatment targeting EGFR has demonstrated high therapeutic efficacy in the clinic [5–7]. However, treatment response is always achieved only in patients with cancer with high EGFR expression.

Traditional computed tomography (CT) and magnetic resonance imaging (MRI) in tumor diagnosis and staging mainly reveal anatomic changes. The expression of specific molecules in a tumor is difficult to demonstrate. Single photon emission computed tomography/computed tomography (SPECT/CT) based on immunological probes (immuno-SPECT/CT) is a common noninvasive molecular imaging method that utilizes a radiolabeled antibody to visualize a specific marker [8–10]. The therapeutic effect of EGFR targeted treatment depends highly on the EGFR expression of the tumor. Although pathological results are the gold standard, the means of obtaining samples are typically invasive and inconvenient. Cetuximab (Cet), a US Food and Drug Administration (FDA)–approved mAb, is widely used for treating digestive tumors with high EGFR expression. However, noninvasive methods that can efficiently classify patients with high-EGFR expression tumors for intensive EGFR targeted treatment are rare.

The intact antibody commonly has a molecular weight of about 150 kDa, which makes its metabolism in the blood very slow (its biological half-life $T_{1/2}$ is always >3 days) [11]. Therefore, it presents significant radiation problems for nuclear medicine immunoinaging. Enzymatic digestion can produce F(ab)$'$$_2$ fragments (about 100 kDa) from an intact antibody to reduce the molecular weight but nevertheless retain the antigen-binding site and immunological binding activity of the intact antibody [9, 12]. In the present study, we fabricated $^{99m}$Tc-labeled cetuximab F(ab)$'$$_2$ fragments (Cet-F(ab)$'$$_2$) as a probe for biodistribution and SPECT/CT imaging assessment of the EGFR expression in murine models of digestive tumors.

2. Materials and Methods

2.1. Cell Culture. HT29 human colon cancer and MGC803 human stomach tumor cell lines were from Shanghai Zhong Qiao Xin Zhou Biotechnology Co., Ltd. (Shanghai, China) and incubated in Dulbecco’s Modified Eagle’s Medium (Servicebio, Wuhan, China) containing 10% heat-inactivated fetal bovine serum (FBS, Gibco, Waltham, MA, USA).

2.2. Mice and Reagents. All animal studies were conducted in accordance with protocols approved by the Animals Ethics Committee of Zhongshan Hospital, Fudan University. Eight-week-old male BALB/c nude mice (20–22 g) were from Charles River (Beijing, China). Anti-EGFR mAb (#ab52894) was from Abcam (Cambridge, UK). Horseradish peroxidase conjugated goat anti-rabbit IgG (H + L) (#GB23303), Cy3-conjugated goat anti-rabbit IgG (H + L) (#GB21303), and DAPI (#G1012) were from Servicebio (Wuhan, China). Anti-$\beta$-actin mAb (#4970) was from Cell Signaling Technologies (Boston, MA, USA). Cetuximab (#A2000) was from Selleck (Shanghai, China). Immunoglobulin G-degrading enzyme of Streptococcus pyogenes (Ides) protease (#20412ES84) was from Yeasen (Shanghai, China).

2.3. Western Blotting. The MGC803 and HT29 cells were seeded in 6-well plates and grown to 70% confluence. The cells were lysed using radioimmunoprecipitation assay lysis buffer plus 1 mM PMSF (Servicebio, Wuhan, China) at 4°C for 30 min. The supernatant was collected, and the protein concentration was quantified by a spectrophotometer. Then, the proteins were denatured with protein loading buffer at 100°C for 10 min. Total protein (20 μg) was loaded into gels (EpiZyme, Shanghai, China) with Muticolor Prestained Protein Ladder (EpiZyme, Shanghai, China). Electrophoresis was performed at 80 V for 30 min and then 120 V for 60 min. All proteins were then transferred to a PVDF membrane. The membrane was blocked with skim milk (5%) blocking buffer for 2 h at room temperature (20°C) and incubated overnight at 4°C with rabbit anti-EGFR antibodies (1:1000 dilution, Abcam) and rabbit anti-$\beta$-actin mAb (1:10,000 dilution, Cell Signaling Technology). Next, the membrane was washed three times with TBS-Tween 20 and incubated with goat anti-rabbit IgG antibodies (1:5000, Servicebio, Wuhan, China) for 2 h at room temperature. The washed membrane was scanned and quantitatively analyzed using a Tanon 4200 imaging system (Tanon, Shanghai, China). The EGFR expression was analyzed and normalized to $\beta$-actin protein for comparison between the MGC803 and HT29 cells using ImageJ 1.44p (National Institutes of Health, Bethesda, MA, USA).

2.4. Preparation of Cet-F(ab)$'$$_2$. Cetuximab was incubated with Ides protease for 30 min at 37°C in digestion buffer (50 mM sodium phosphate, 150 mM NaCl, pH 6.6). The digested products were incubated with protein A beads for 1 h and centrifuged. The Fc portion attached to the beads was removed in the sediment while the purified Cet-F(ab)$'$$_2$ remained in the supernatant. The Cet-F(ab)$'$$_2$ and cetuximab were evaluated by sodium dodecyl sulfate-polyacrylamide gel electrophoresis (SDS-PAGE) on a 4–15% gel under 150 V for 1 h. The stability of Cet-F(ab)$'$$_2$ in PBS and 1%BSA was evaluated through SDS-PAGE.

2.5. Immunocytochemistry. Cet-F(ab)$'$$_2$ and cetuximab were conjugated with 5(6)-carboxytetramethylrhodamine succinimidyl ester (5(6)-TAMRA, Xi’an Ruixi Biological Technology, Xi’an, China) for 2 h, with a 1:3 molar ratio of Cet-F(ab)$'$$_2$ to 5(6)-TAMRA/cetuximab to 5(6)-TAMRA in carbonate buffer (pH 9.0). The fluorescent product was purified using PD-10 columns by removing excess dye. After MGC803 cells had been cultured in 6-well plates at 40% confluence, they were incubated with 66.67 nmol/L TAMRA-Cet-F(ab)$'$$_2$ or TAMRA-cetuximab overnight. Images were captured using an Olympus imaging system (Olympus, Tokyo, Japan).

2.6. Preparation of $^{99m}$Tc-MAG3-Cet-F(ab)$'$$_2$. Figure 1 shows the synthetic route of $^{99m}$Tc-MAG3-Cet-F(ab)$'$$_2$. In brief,
Cetuximab was incubated with MAG3 for 2 h at room temperature in carbonate buffer (pH 9.0). The molar ratio of cetuximab to MAG3 was 1:5, according to previous described methods [13–15]. The MAG3-Cet was purified using a Zeba Spin Desalting Column 7 K MWCO (Thermo Fisher Scientific, Waltham, MA, USA). MAG3-Cet-F(ab′)2 was prepared using IdeS protease and purified by removing the Fc portion using protein A beads (Epizyme Biomedical Technology, Shanghai, China). Figure S1 shows the characterization of MAG3-Cet and MAG3-Cet-F(ab′)2 by SDS-PAGE (Supplementary File). The cheator-to-antibody ratio of the product was determined by liquid chromatography-mass spectrometry (LC-MS) (Bioaccord, Waters, Milford, USA). In brief, MAG3-Cet was incubated with IdeS protease for 30 min at 37°C in digestion buffer (50 mM sodium phosphate, 150 mM NaCl, pH 6.6). The digested products were incubated with protein A beads for 1 h and centrifuged. The Fc portion attached to the beads was removed in the sediment while the purified MAG3-Cet-F(ab′)2 remained in the supernatant. Size-exclusion high performance liquid chromatography (SEC-HPLC) was performed to determine the radio purity of the product using an Agilent 1260 Infinity II Bio-Inert System (Agilent, Santa Clara, USA) with a Tosoh Bioscience TSK gel (G3000SWXL, 7.8 mm × 300 mm) at 20°C and a Bioscan B-FC-1000 radiation detector (energy range: 0–20 M cpm, Eckert & Ziegler Group, Hopkinion, USA). The mobile phase was PBS (pH 7.4). The flow rate was set at 0.5 mL/min. Sample was detected at 220 nm with a UV detector. For 99mTc labeling, 100 μg MAG3-Cet-F(ab′)2 was added to a combined solution of 45 μL ammonium acetate (0.25 M) and 15 μL tartrate buffer, and then no more than 25 μL (approximately 5 mCi) 99mTc-pertechnetate generator eluate was added. Immediately after vortexing, 3 μL freshly prepared 1 mg/mL SnCl2·2H2O solution was added. The combined solution was incubated at room temperature in carbonate buffer (pH 9.0). The molar ratio of cetuximab to MAG3 was 1:5, according to previous described methods [13–15]. The MAG3-Cet was purified using a Zeba Spin Desalting Column 7 K MWCO (Thermo Fisher Scientific, Waltham, MA, USA). MAG3-Cet-F(ab′)2 was prepared using IdeS protease and purified by removing the Fc portion using protein A beads (Epizyme Biomedical Technology, Shanghai, China). Figure S1 shows the characterization of MAG3-Cet and MAG3-Cet-F(ab′)2 by SDS-PAGE (Supplementary File). The cheator-to-antibody ratio of the product was determined by liquid chromatography-mass spectrometry (LC-MS) (Bioaccord, Waters, Milford, USA). In brief, MAG3-Cet was incubated with IdeS protease for 30 min at 37°C in digestion buffer (50 mM sodium phosphate, 150 mM NaCl, pH 6.6). The digested products were incubated with protein A beads for 1 h and centrifuged. 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The combined solution was incubated at room
temperature for 1 h under vortexing. $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$ was purified from unlabeled reduced $^{99m}\text{Tc}$ with PD-10 desalting columns. Radio-HPLC was performed to determine the radiochemical purity of $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$ with the same machine, mobile phase, and flow rate as mentioned above.

2.7. Stability, Competition and Binding Assay of $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$. The stability of $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$ was determined in 1x phosphate-buffered saline (PBS) and 1% bovine serum albumin (BSA) for 1, 6, 12, and 24 h. The unfolding agent was a 1:2 (v/v) mixture of 0.9% saline and methanol. For the competition assay, $2 \times 10^5$ MGC803 cells were seeded in 24-well plates with 1.25-1280 nM unlabeled cetuximab and 10 nM $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$ and incubated at 37°C for 60 min. The supernatant was discarded, and the cells were washed twice with ice-cold PBS and harvested for determination of radioactivity using a gamma counter. For the binding assay, $2 \times 10^5$ MGC803 cells and HT29 cells each were seeded in 24-well plates. $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$ (0.1-4 nM) in PBS solution was added to the plates and incubated at room temperature for 1 h, then the supernatant was discarded while the cells were washed twice with ice-cold PBS and harvested for determination of radioactivity. The binding results including the maximum binding ability ($B_{\text{max}}$) and the dissociation constant ($K_d$) were obtained via GraphPad Prism (GraphPad Inc., La Jolla, CA, USA).

2.8. Mouse Model Preparation. All animal studies were performed in accordance with protocols approved by the Animals Ethics Committee of Zhongshan Hospital, Fudan University. Subcutaneous MGC803 and HT29 tumors were induced in 6-week-old male nude mice by injecting their lower right flanks with $1 \times 10^6$ tumor cells suspended in 200 μL PBS. The tumors were monitored every other day.

2.9. Biodistribution and Micro-SPECT/CT Imaging. The MGC803 tumor-bearing mice ($n = 16$) were injected with $18.5$ MBq (50 μg) $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$. After 1, 6, 12, and 24 h, four mice from each group were sacrificed and dissected. Tumors, blood, and major tissues/organs (including heart, lung, liver, kidney, spleen, colon, stomach, bone, and muscle) were harvested and weighed. Sample tissue radioactivity was measured using a gamma counter. The radioactivity concentration of the tissue was expressed as the percentage injected dose per g (%ID/g), and the tumor to muscle (T/M) ratio was defined as the ratio of radioactivity that had accumulated in tumors to that in the contralateral muscle. The experiments were repeated three times.

Micro-SPECT/CT scanning was conducted using a Nano SPECT/CT scanner (BioScan, Washington DC, USA). $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$ (18.5 MBq/50 μg/mouse) was injected into tumor-bearing mice via the tail vein. After 16 h, the mice were anesthetized via 2% isoflurane inhalation. CT was performed first with the following parameters: frame resolution, $256 \times 512$; tube voltage, $45$ kVp; current, $0.15$ mA; and exposure time, $500$ ms/frame. Each scan spanned about 7 min. SPECT was performed after CT scanning with same bed position and the following parameters: four high-resolution conical collimators with 9-pinhole plates; energy peak, $140$ keV; window width, $10%$; resolution, $1$ mm/pixel; matrix, $256 \times 256$; and scan time, $70$ s/projection, 24 projections in all. Each mouse was scanned in 42 minutes on average. Three-dimensional ordered-subset expectation maximization images were reconstructed using the HiSPECT algorithm. Reconstructed SPECT/CT data were transferred to InVivoScope (Version 1.43, BioScan) for postprocessing.

2.10. Immunofluorescence. After deparaffinization and hydration, the HT29 and MGC803 tumor slices were incubated in 5% BSA in PBS buffer for 1 h. The slices were incubated in rabbit anti-EGFR antibody (1:200) overnight at 4°C. After washing in PBS, the slices were stained with CY3-conjugated goat anti-rabbit antibody (1:100) for 1 h. Following three PBS washes, the nuclei were stained using DAPI. Images were captured using an Olympus imaging system.

2.11. Statistical Analysis. Data are presented as the means ± standard deviation (SD) derived from at least three independent experiments. The Student t-test was applied for intergroup comparisons using GraphPad Prism. All tests were 2-sided, and a statistical P value of <0.05 was considered statistically significant.

3. Results

3.1. MGC803 and HT29 Cell EGFR Expression Levels. The EGFR expression in MGC803 cells and HT29 cells was quantified by western blotting. MGC803 cells had a significantly higher relative expression ratio of EGFR/β-actin than HT29 cells in vitro (1.21 ± 0.10 vs. 0.13 ± 0.02, P < 0.01) (Figure 2(a)). Immunocytochemistry showed stronger fluorescence intensity in MGC803 cells, which was consistent with western blotting results (Figure 2(b)).

3.2. Molecular Weight, Binding Affinity, and Stability of Cet-F(ab′)$_2$ SDS-PAGE showed that the molecular weight of Cet-F(ab′)$_2$ and cetuximab was about 100 kDa and 150 kDa, respectively (Figure 3(a)). Fluorescence microscopy showed that TAMRA-Cet-F(ab′)$_2$ had similar binding affinity for MGC803 cells compared with TAMRA-Cet (Figure 3(b)). SDS-PAGE showed that Cet-F(ab′)$_2$ had excellent stability following incubation in PBS or 1%BSA, with >90% remained intact until 24 h (Figure 3(c)).

3.3. Successful Preparation of MAG$_3$-Cet-F(ab′)$_2$ and $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$. Characterization of successful MAG$_3$-Cet-F(ab′)$_2$ preparation using HPLC is shown in Figure 4. The overall conjugation ratio of MAG$_3$ per Cet-F(ab′)$_2$ identified by LC-MS was about 0.74 (Figure S2). Characterization of $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$ using SDS-PAGE can be found in Figure S3. As identified by SEC-HPLC, the radio purity $^{99m}\text{Tc}$-MAG$_3$-Cet-F(ab′)$_2$ before purification about 82.2%. After purification with PD-10 desalting column, the radiochemical purity was about
93.63% (Figure 5(a)). The specific activity and radioactive concentration of the final preparation were 1.48 MBq/μg and 296 MBq/mL, respectively. The $^{99m}$Tc-MAG$_3$-Cet-F(ab$'$)$_2$ had excellent stability, with >90% remaining intact over 24 h in both normal saline (NS) and 1% BSA (Figure 5(b)). The competition binding assay showed that $^{99m}$Tc-MAG$_3$-Cet-F(ab$'$)$_2$ had excellent specificity for MGC803 tumor cells (Figure 5(c)). Unlabeled cetuximab with >1000-fold concentration almost blocked $^{99m}$Tc-MAG$_3$-Cet-F(ab$'$)$_2$ binding to MGC803 tumor cells (<3%). The fabricated $^{99m}$Tc-MAG$_3$-Cet-F(ab$'$)$_2$ presented higher affinity to the MGC803 cells with a higher $B_{\text{max}}$ ($5.68 \times 10^{-19}$ mol ligands/cell) and a lower $K_d$ (0.6147 nM), compared to the HT29 cells ($B_{\text{max}} = 1.66 \times 10^{-19}$ mol ligands/cell, $K_d = 1.008$ nM). These results suggest that MGC803 cells had both higher total EGFR expression level and Cet-F(ab$'$)$_2$ binding affinity than HT29 cells.

3.4. In Vitro Biodistribution, SPECT/CT Imaging, and Immunofluorescence. To quantify $^{99m}$Tc-MAG$_3$-Cet-F(ab$'$)$_2$ uptake at 1, 6, 16, and 24 h after injection, the MGC803 tumor-bearing mouse models underwent in vitro biodistribution studies. $^{99m}$Tc-MAG$_3$-Cet-F(ab$'$)$_2$ uptake in the MGC803 tumors at 1, 6, 16, and 24 h postinjection was $4.28 \pm 1.04$, $8.00 \pm 0.39$, $13.51 \pm 2.17$, and $4.46 \pm 0.80$%ID/g, respectively, and the T/M ratios were $3.40 \pm 1.59$, $5.97 \pm 0.75$, $17.29 \pm 5.72$, and $11.33 \pm 2.62$, respectively (Figure 6(a)). At 16 h, the $T/L$ (tumor to liver), $T/K$ (tumor to kidney), and $T/B$ (tumor to blood) ratios were significantly higher than the corresponding results at 1 h ($0.18 \pm 0.07$, $0.15 \pm 0.05$, $0.25 \pm 0.10$, respectively), 6 h ($0.98 \pm 0.15$, $0.95 \pm 0.05$, $1.29 \pm 0.26$, respectively), and 24 h ($1.09 \pm 0.09$, $0.83 \pm 0.13$, $1.15 \pm 0.09$, respectively), respectively. These results indicate that $^{99m}$Tc-MAG$_3$-Cet-F(ab$'$)$_2$ was mainly metabolized by the liver and kidney. Background radioactivity in the stomach, colon, and bone was minimal, which was in agreement with the imaging data. The SPECT/CT imaging (Figure 6(b)) of the subcutaneous tumors demonstrated significantly increased radioactivity accumulation in the MGC803 tumor (high EGFR expression) than in the HT29 tumor (low EGFR expression) ($T/M$: $3.21 \pm 0.27$ vs. $1.09 \pm 0.07$, $P < 0.05$). Immunofluorescence showed that the MGC803 tumor slices
had stronger fluorescence intensity than the HT29 tumor slices, which was consistent with the western blotting and immunocytochemistry results (Figure 6(c)). Spearman correlation analysis clarified the relationship between the T/M ratio on SPECT/CT imaging and the integrated density/area (IntDen/Area) on immunofluorescence ($R^2 = 0.9473, P < 0.01$, Figure 6(d)). These results indicate that $^{99m}$Tc-MAG$_3$-Cet-F(ab$'$)$_2$ is a good tracer for targeting the EGFR expression in tumors.

4. Discussion

EGFR is widely expressed in nearly every cancer type, and its high expression in tumors correlates with poor patient outcome [16]. Several studies have demonstrated that patients with digestive tumors benefited from EGFR-targeted therapy using cetuximab [17–19]. For patients with unresectable tumors, it is difficult to evaluate the EGFR expression through pathology. Therefore, noninvasive evaluation of the EGFR expression is particularly important. Cetuximab, an EGFR inhibitor widely used in clinical practice, is suitable for noninvasive evaluation of the EGFR expression [20, 21]. Immuno-SPECT combines the high specificity of antibodies with the high sensitivity of SPECT imaging [22, 23]. Compared with PET, one advantage of SPECT is the price. Typically, achieving the best imaging contrast for a radionuclide-labeled intact antibody (about 150 kDa) requires $\geq 48$ h [8, 10, 24]. Therefore, this renders it
Figure 4: The HPLC results showing ultraviolet profiles of MAG3-Cet, MAG3-Cet-F(ab')2 and MAG3-Cet-Fc. (a) The HPLC result of MAG3-Cet. (b) The HPLC result of MAG3-Cet-F(ab')2 and MAG3-Cet-Fc after digesting MAG3-Cet with IdeS protease. (c) The HPLC result of the mixture from (b) but after reaction with protein A beads. The residual MAG3-Cet and most of the MAG3-Cet-Fc were removed by protein A beads. (d) The HPLC result of the mixture of (a) and (c).
unsuitable for imaging radionuclides with short half-lives. For example, for $^{99m}$Tc ($T_{1/2} \approx 6\text{ h}$), which is most widely used in SPECT imaging, it would be impossible to achieve the best imaging time before dramatic decay when labelling an intact antibody. If a nuclide with a long half-life was used for labelling an intact antibody, which would allow achievement of the best imaging time (>48 h) before dramatic decay, issues regarding high radiation caused by delayed peak tumor uptake and slow clearance would arise, which would hinder the clinical translation. Regarding the radiation issue, the pretargeting imaging strategy is advantageous, allowing the injection of modified mAbs first with a...
predictable duration for its accumulation to the target site. Then, a small molecule radioligand that can conjugate to the pretargeted mAb is injected for imaging while the redundant radioligand is cleared quickly [25, 26]. The most promising pretargeting methodology is based on inverse electron demand \((4+2)\) Diels-Alder (IEDDA) cycloaddition between 1,2,4,5-terazine (Tz) and transcyclooctene (TCO), which has been widely used in tumor imaging studies [26, 27]. Recently, the Tz/TCO-based and cetuximab pretargeted imaging strategy was successfully used for assessing the EGFR expression in colorectal cancer [28]. However, the expensive cost of synthesizing the Tz and TCO molecules and the inconvenience caused by two injections hinder its clinical use. Therefore, the synthesis of a new probe with high specificity and relatively small molecular weight is necessary.

van Dijk et al. [29, 30] prepared Cet-F(ab\(^\prime\))\(_2\) fragment through pepsin digestion and successfully used it for the imaging EGFR expression of head and neck cancer. Here, we used the IdeS digestion to obtain the Cet-F(ab\(^\prime\))\(_2\), which is entirely different from pepsin digestion. Compared with pepsin, IdeS is a unique cysteine protease that digests antibodies at a single amino acid site below the hinge region, which is suitable for antibodies from multiple sources (e.g., human, mouse, rabbit, monkey, sheep, chimeric IgG, and Fc fusion protein), with high specificity and rapid reaction time (within 30–60 minutes). van Dijk et al. [29] used pepsin to obtain Cet-F(ab\(^\prime\))\(_2\) required with a longer reaction time (4 h) and stricter reaction conditions (pH = 3.8). In addition, pepsin would digest many more restriction sites compared to IdeS [31, 32].

The molecular weight of Cet-F(ab\(^\prime\))\(_2\) is about 100 kDa, which is smaller and therefore leads to quicker clearance, compared to its intact counterpart. Yamaguchi et al. [24] and Perk et al. [33] found that the best imaging time point for intact cetuximab-targeted imaging was 48–72 h, which they confirmed with biodistribution assay and PET imaging. In contrast, the best time point of \(^{99m}\)Tc-MAG\(_2\)-Cet-F(ab\(^\prime\))\(_2\)-based imaging as identified through biodistribution assay in the present study was 16 h. Although the molecular weight of Cet-F(ab\(^\prime\))\(_2\) is smaller, its unique properties make it a promising candidate for pretargeted imaging.
weight was reduced only by approximately one-third (150 kDa to 100 kDa), the clearance rate was significantly improved. Therefore, $^{99m}$Tc is suitable for labeling this tracer, which would certainly reduce patient radiation exposure if translated to the clinic in the future. In addition, immunocytochemistry and SDS-PAGE showed that the Cet-F(ab$\prime$)$_2$ had similar ability to intact cetuximab to bind to EGFR on tumor cells. Furthermore, the Cet-F(ab$\prime$)$_2$ had excellent stability in both NS and 1% BSA. In vitro, the Western blotting and the immunocytochemistry assays revealed higher expression of EGFR on the MGC803 cells than the HT29 cells, while the fabricated $^{99m}$Tc-MAG$_3$-Cet-F(ab$\prime$)$_2$ presented higher affinity to the MGC803 cells with a higher $B_{\text{max}}$ ($5.68 \times 10^{-19}$ mol ligands/cell) and a lower $K_d$ (0.6147 nM), compared to the HT29 cells ($B_{\text{max}} = 1.66 \times 10^{-19}$ mol ligands/cell, $K_d = 1.008$ nM). These results indicated a good affinity and targeting ability of $^{99m}$Tc-MAG$_3$-Cet-F(ab$\prime$)$_2$ to EGFR. The biodistribution studies showed that the $T/M$ ratio peaked at approximately 17.29 ± 5.72 at 16 h after $^{99m}$Tc-MAG$_3$-Cet-F(ab$\prime$)$_2$ injection. Therefore, we consider 16 h the best imaging time point. In SPECT/CT imaging, the MGC803 tumor had significantly higher $^{99m}$Tc-MAG$_3$-Cet-F(ab$\prime$)$_2$ uptake than HT29 tumor, which was consistent with in vitro results.

5. Conclusion

SPECT/CT imaging using $^{99m}$Tc-MAG$_3$-Cet-F(ab$\prime$)$_2$ showed rapid and sustained high radionuclide-uptake in EGFR-positive digestive tumors with high image contrast, which indicates the potential for noninvasive evaluation of EGFR expression in tumors.

Data Availability

The data used to support the findings of this study are available from the corresponding authors upon reasonable request.

Ethical Approval

All applicable institutional and/or national guidelines for the care and use of animals were followed.

Conflicts of Interest

The authors declare that there is no conflict of interest regarding this article.

Authors’ Contributions

G.L., D.S., and D.C. conceived and designed this study. D.S., Z.X., and Z.S. were involved in synthesizing the probe used in this study. D.S. and Y.Z. performed the experiments. D.S. and G.L. wrote and edited the main manuscript. D.C. and G.L. controlled the quality of this study and received funding for this study. Dai Shi and Yiqiu Zhang contributed equally to this work.

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Supplementary Materials

Supporting data illustrating the formation and characterization of $^{99m}$Tc-MAG$_3$-Cet-F(ab$\prime$)$_2$. Figure S1: image of full SDS-PAGE illustrating the quality control of MAG$_3$-Cet and MAG$_3$-Cet-F(ab$\prime$)$_2$. Figure S2: the LC-MS results of MAG$_3$-Cet and MAG$_3$-Cet-F(ab$\prime$)$_2$. Figure S3: characterization of $^{99m}$Tc-MAG3-Cet-F(ab$\prime$)$_2$. (Supplementary Materials)

References


